

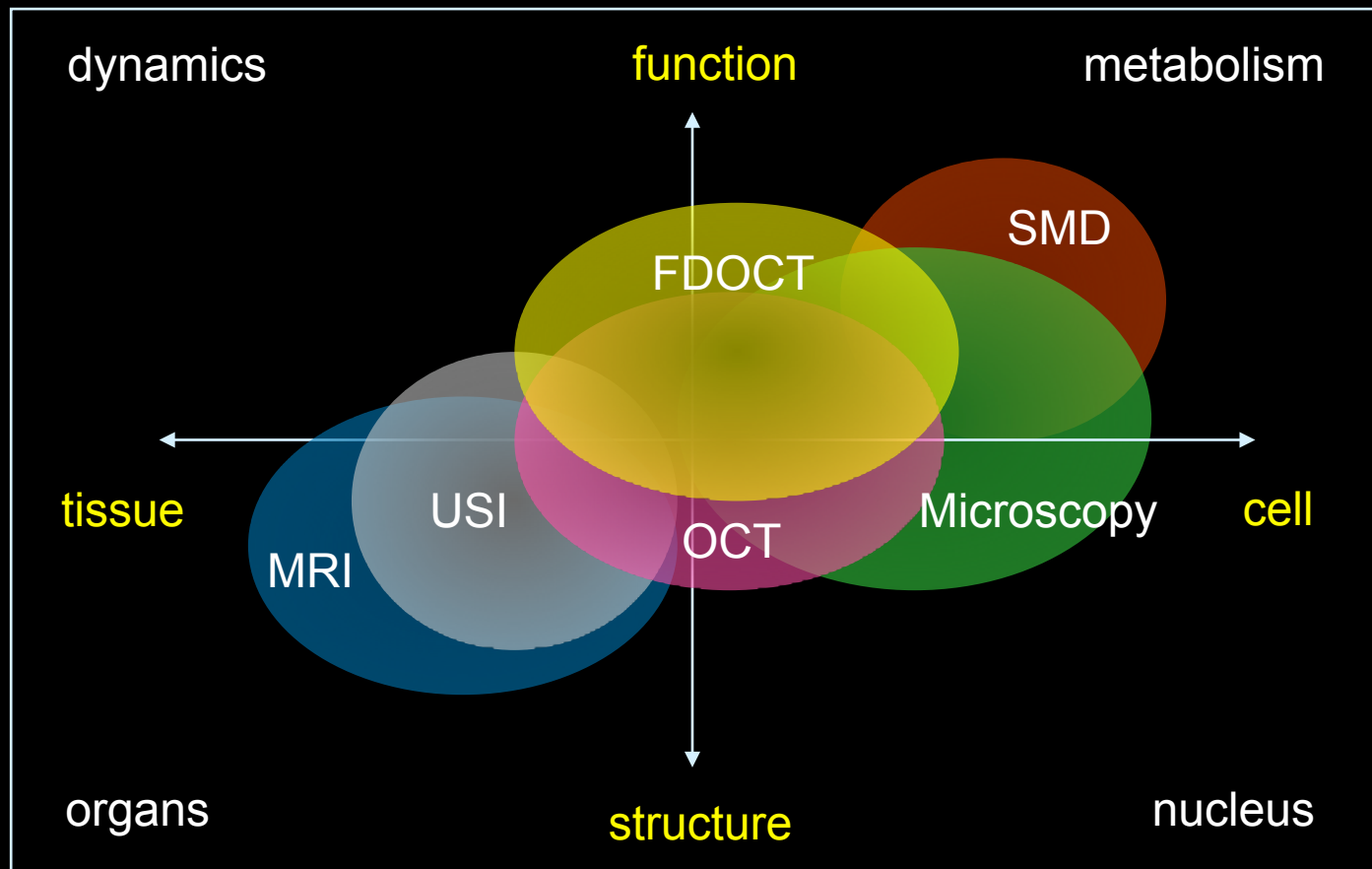


Optical Coherence Tomography

missing link in medical imaging

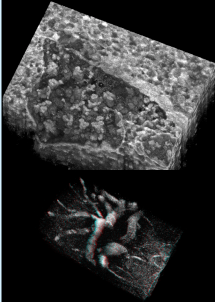
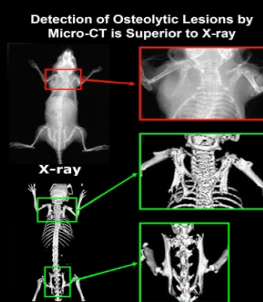
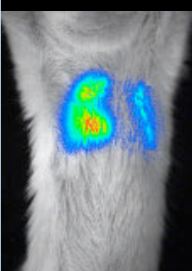
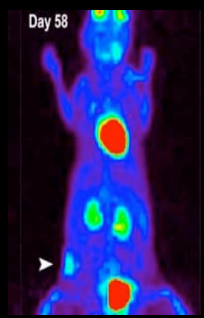
Rainer A. Leitgeb

Center of Biomedical Engineering and Physics - Biomedical Optics Group
Medical University of Vienna,
Währingerstr.13, A-1090 Vienna, Austria



Tomographic Methods



Method	OCT	μ CT	MRI	USI	ODT	PET
<i>Resolution</i>	+++	++	-	-	-	-
<i>Non Hazard</i>	+++	--	++	++	+-	-
<i>Tissue depth</i>	-	+++	+++	++	+	+++
<i>Speed</i>	+++	-	-	++	--	--
<i>Molecular contrast</i>	- +	-	+	--	+++	++
<i>flow</i>	+++	--	- +	++	--	--
		Detection of Osteolytic Lesions by Micro-CT is Superior to X-ray 				Day 58 

En-lightening Information



Property of Light



Intensity

Spectrum

Phase

Polarization

Flourescence

Sample Property

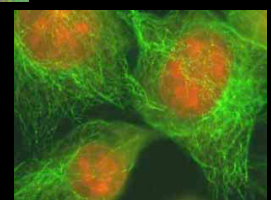
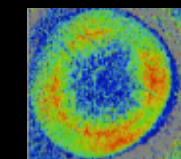
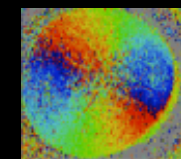
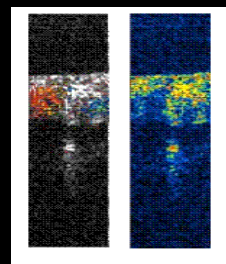
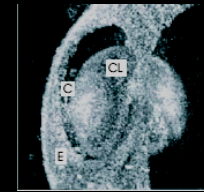
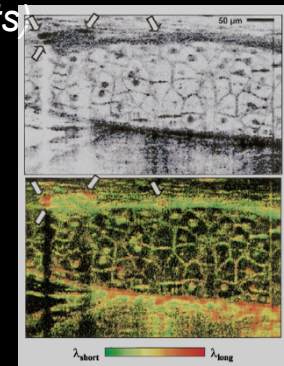
Reflectivity
(refractive index gradients)

Absorption,
Scattering

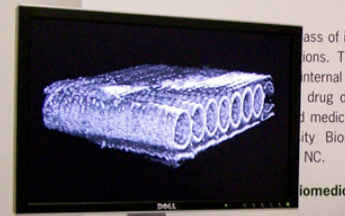
Dispersion,
dynamic structural changes

Retardance,
Rotation

Lifetime, molecular composition



OCT impact



class of in vivo optical
sensors. These systems
internal tissue micro-
structure, drug develop-
ment, and medical
vision. Biophysics
Biomedical Engineering
NC.



1997 1998 1999 2000 2001



Cirrus™ HD-OCT Platform from Carl Zeiss Meditec, Inc.

Media Contact: Amy Cook
amycook@zeiss.com



2003 2004 2005 2006



OCT - Selected Chapters



Structural

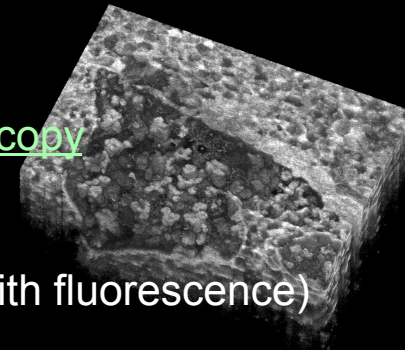
Optical Coherence Tomography

Applications: retinal Imaging, full anterior chamber, endoscopy

Optical Coherence Microscopy with extended focus depth

(endocrine pancreas, mouse breast, brain, combination with fluorescence)

Ultrahigh Speed FDOCT



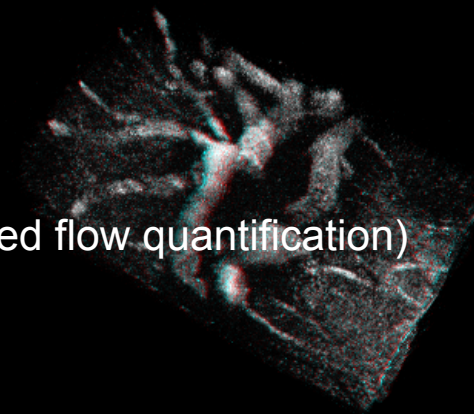
Functional

Doppler μ -Tomography

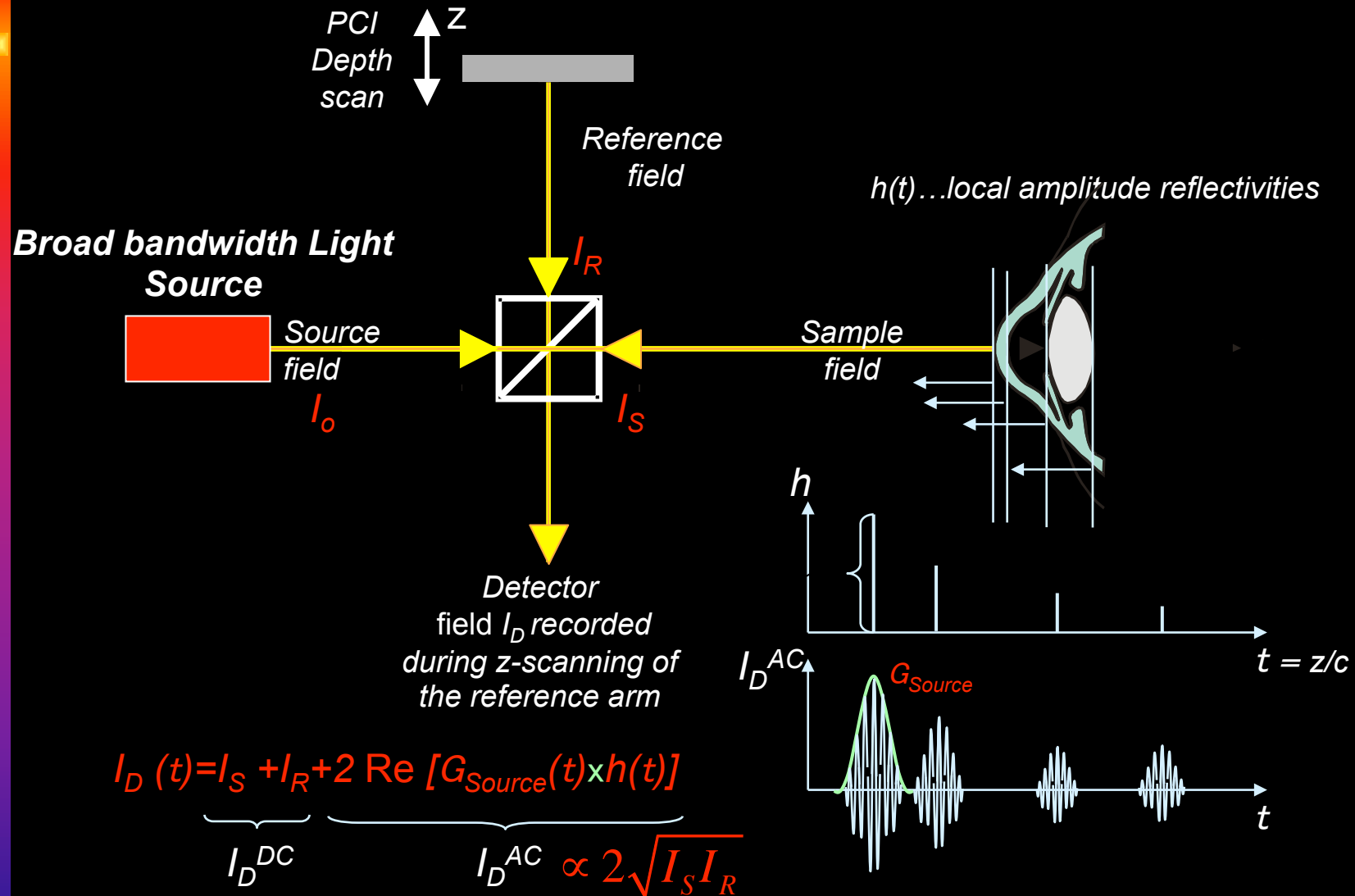
(optical vivisectioning of retinal vessels, intensity based flow quantification)

Optical Testing of Retinal Physiology

(frequency encoded testing of receptor response)



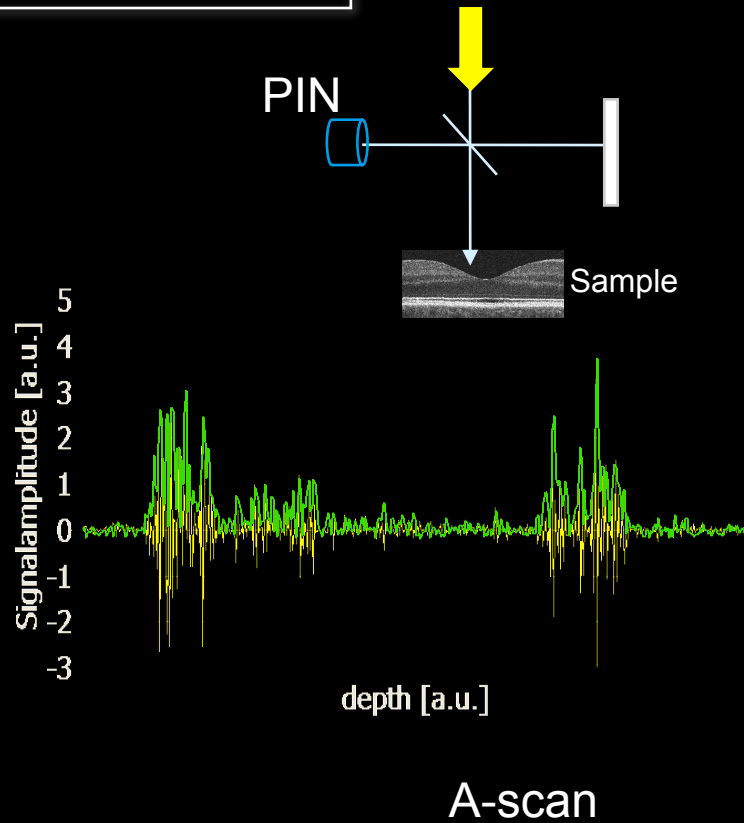
Partial Coherence Interferometry



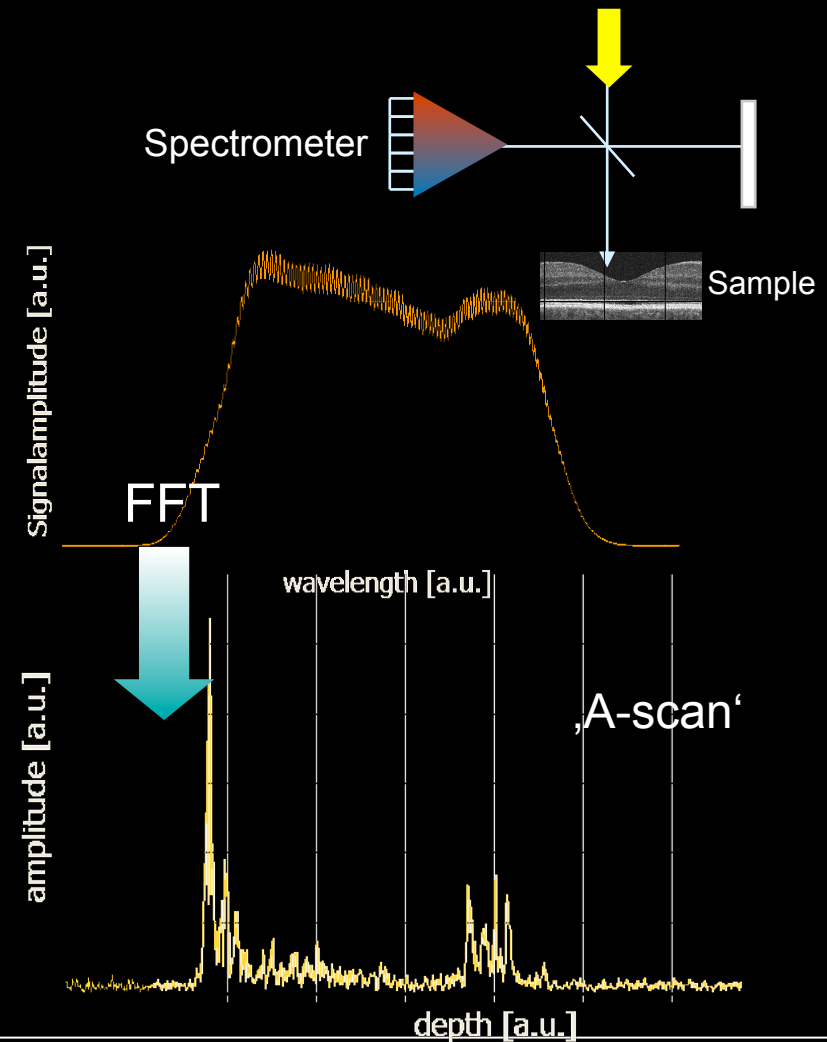
OCT Methods



Time domain



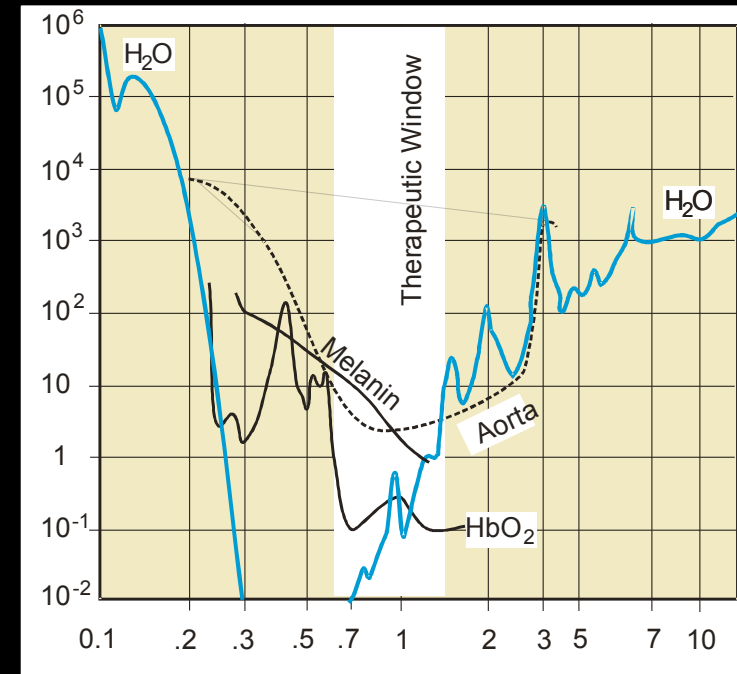
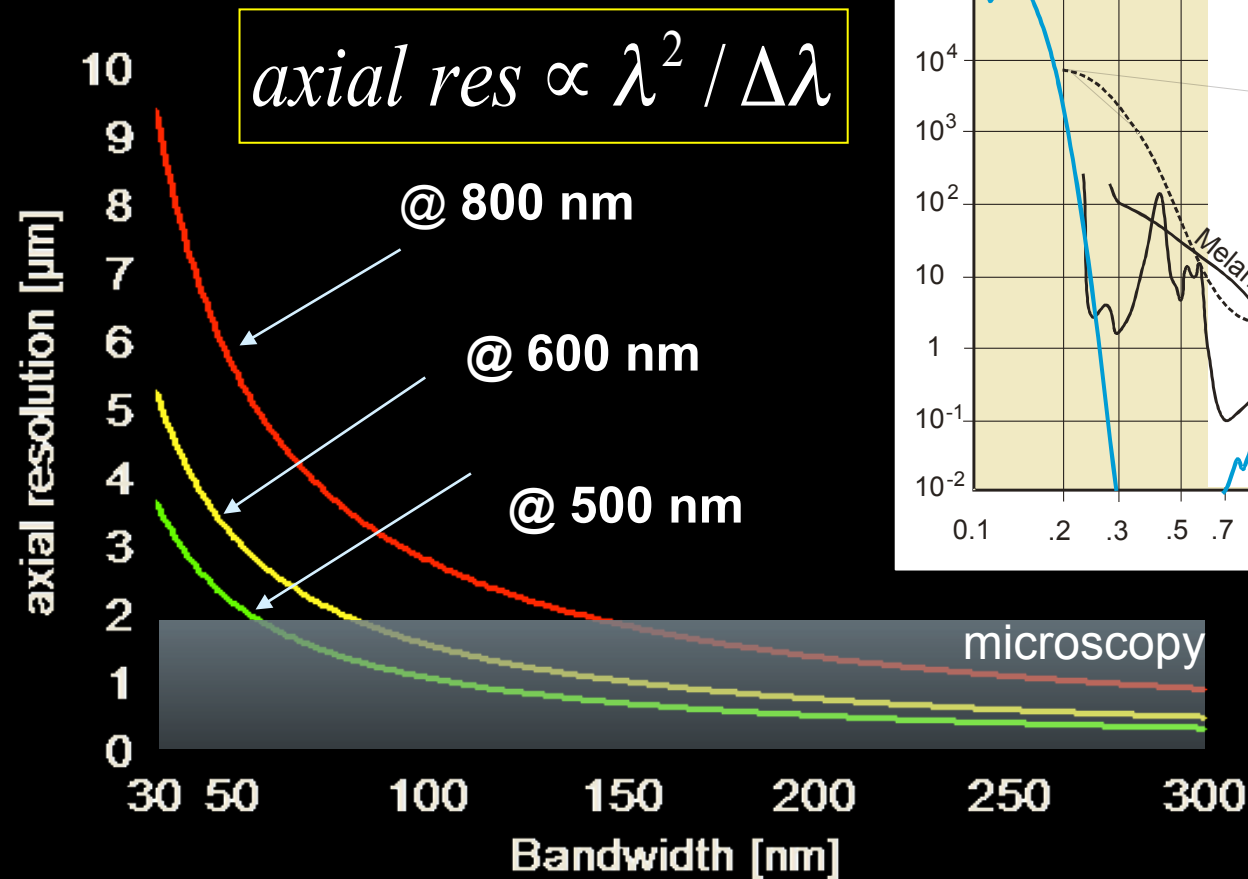
Fourier domain



Resolution



OCM depth resolution is decoupled from transverse resolution



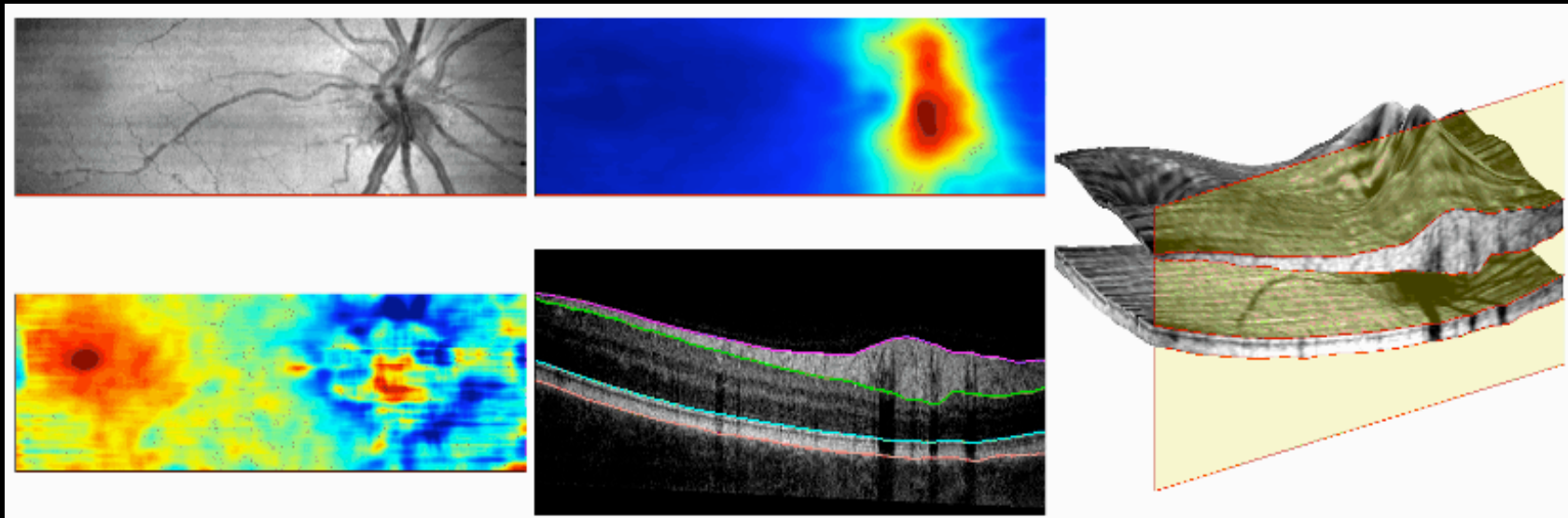
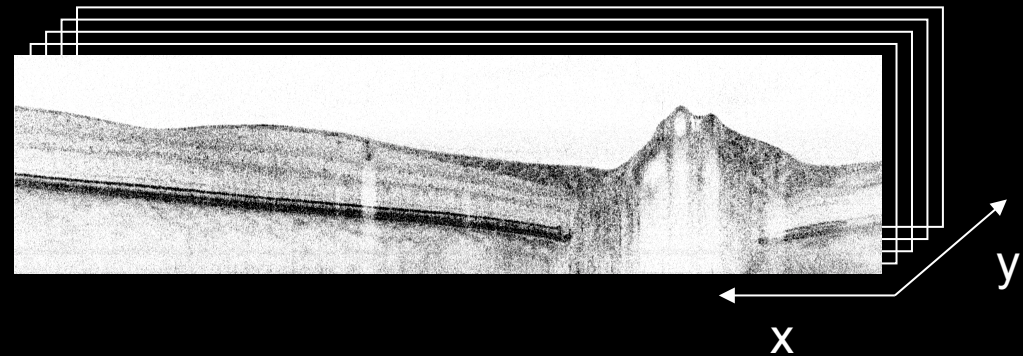
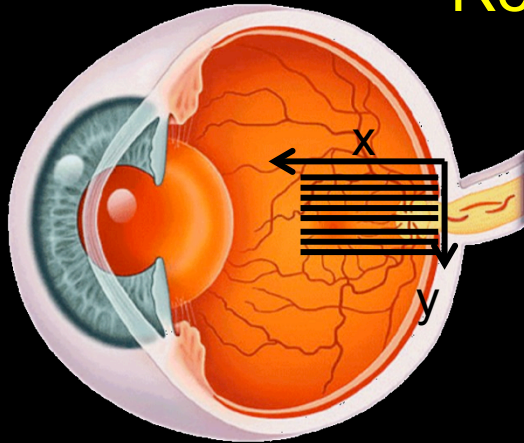
Assumptions: Gaussian Spectrum



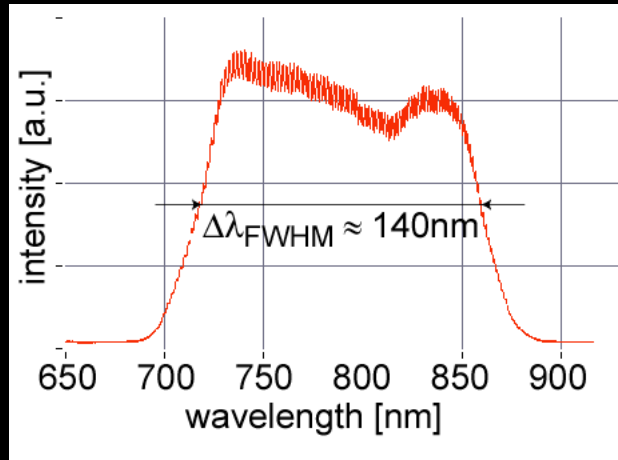
Ophthalmology



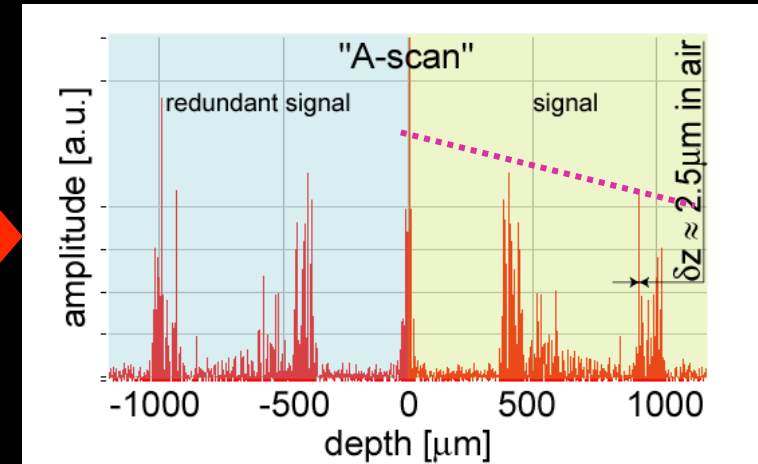
Retinal in-vivo tomography



FDOCT Drawbacks

 $\lambda \rightarrow k$

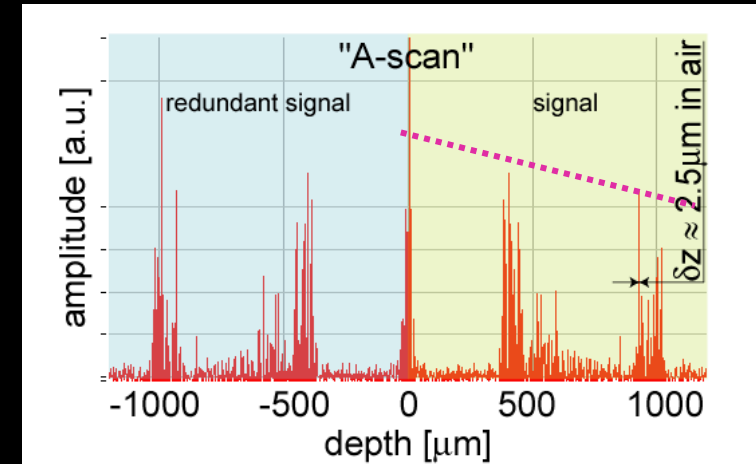
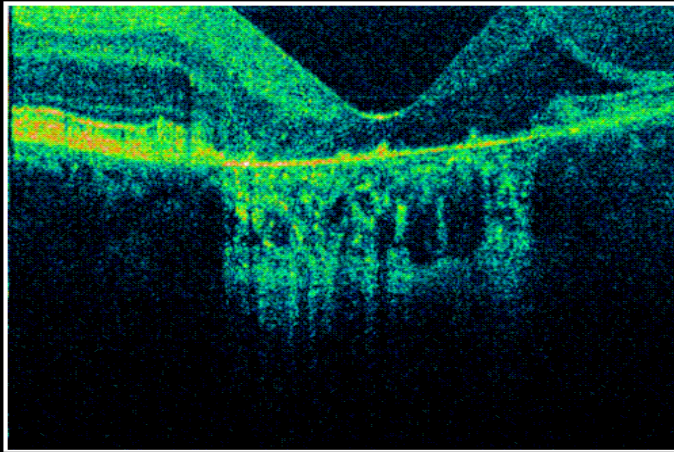
FFT



Main drawbacks (spectrometer-based FDOCT):

- Rigid depth range (sampling by array pixel number)
- Depth dependent sensitivity
- Fringe washout for moving structure
- Mirrored/redundant structure terms

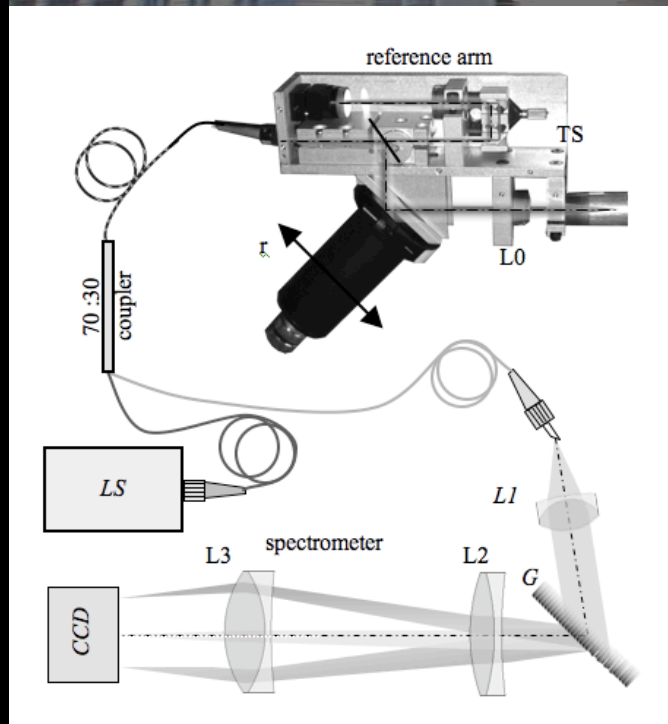
FDOCT Drawbacks



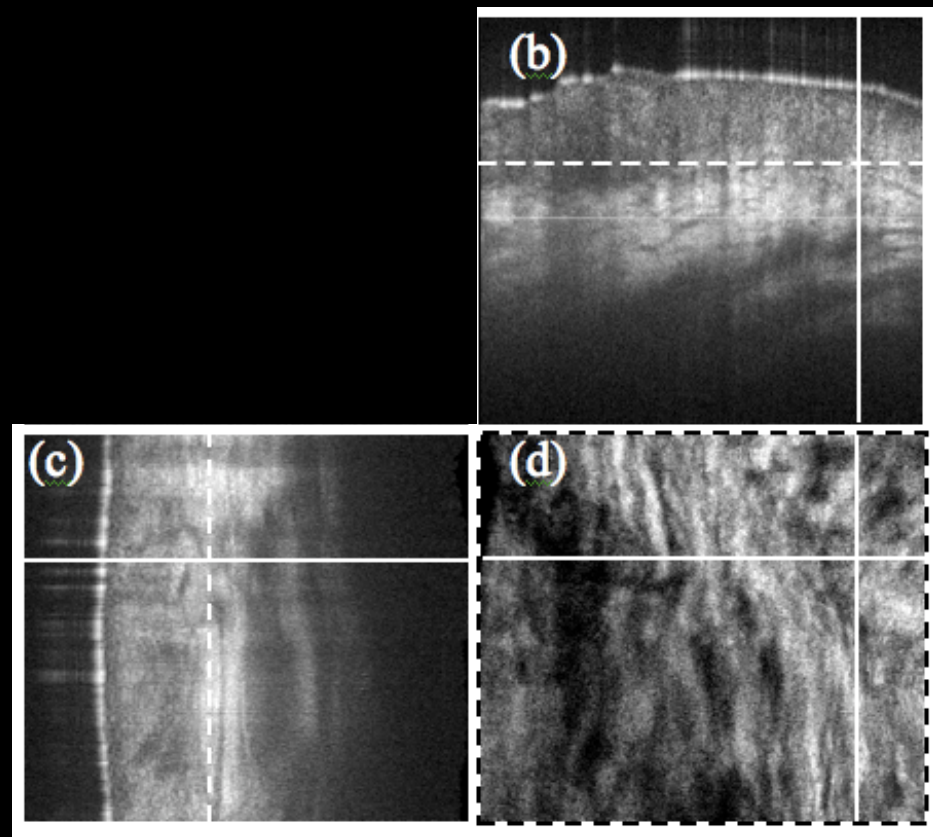
Main drawbacks (spectrometer-based FDOCT):

- Rigid depth range (sampling by array pixel number)
- Depth dependent sensitivity
- Fringe washout for moving structure
- Mirrored/redundant structure terms

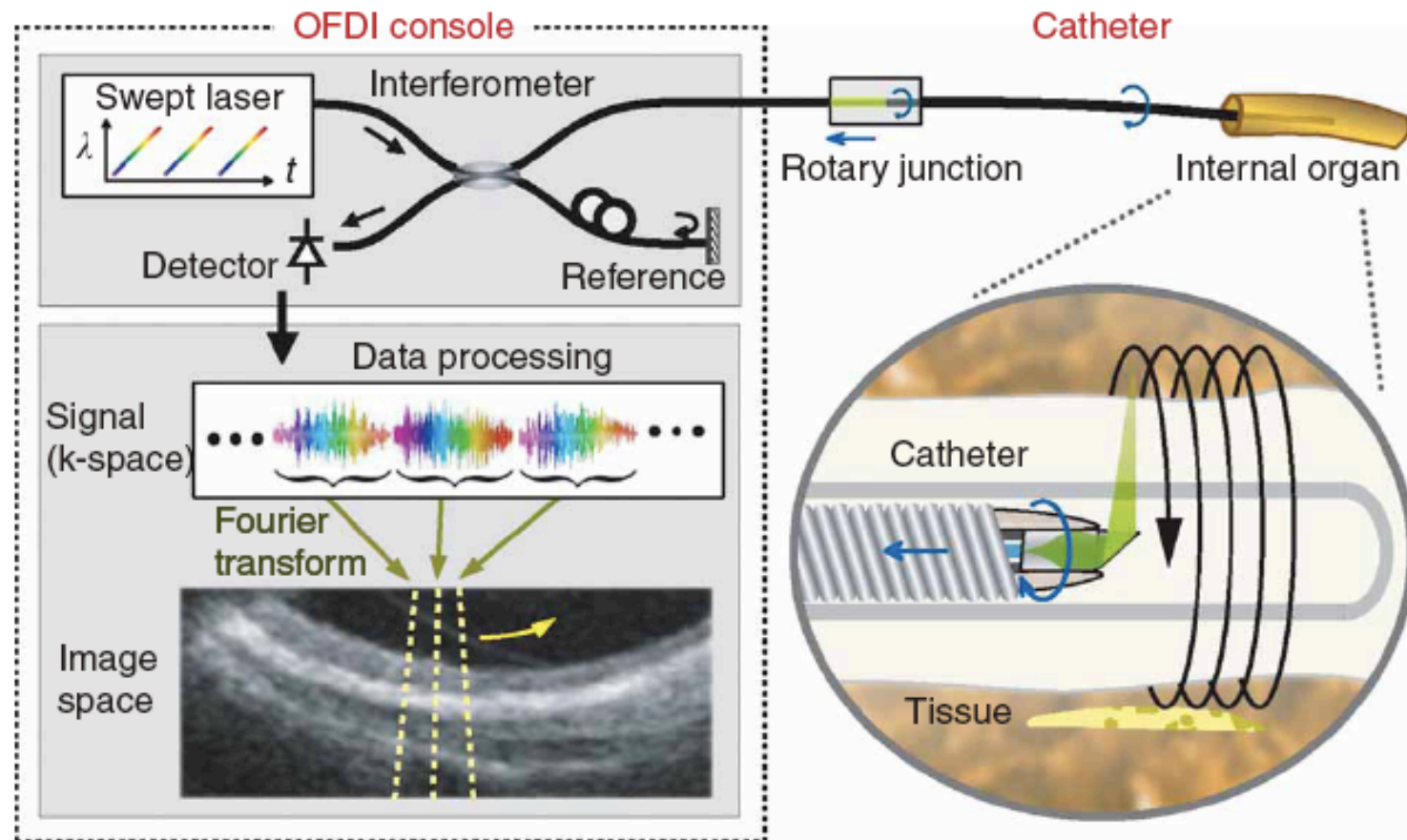
Tissue imaging – Complex Ambiguity



Tomogram of human inner lip (3mm x 2.5mm)
Wavelength 1300nm
Axial resolution 10 μ m



Endoscopic OCT – swept source OCT

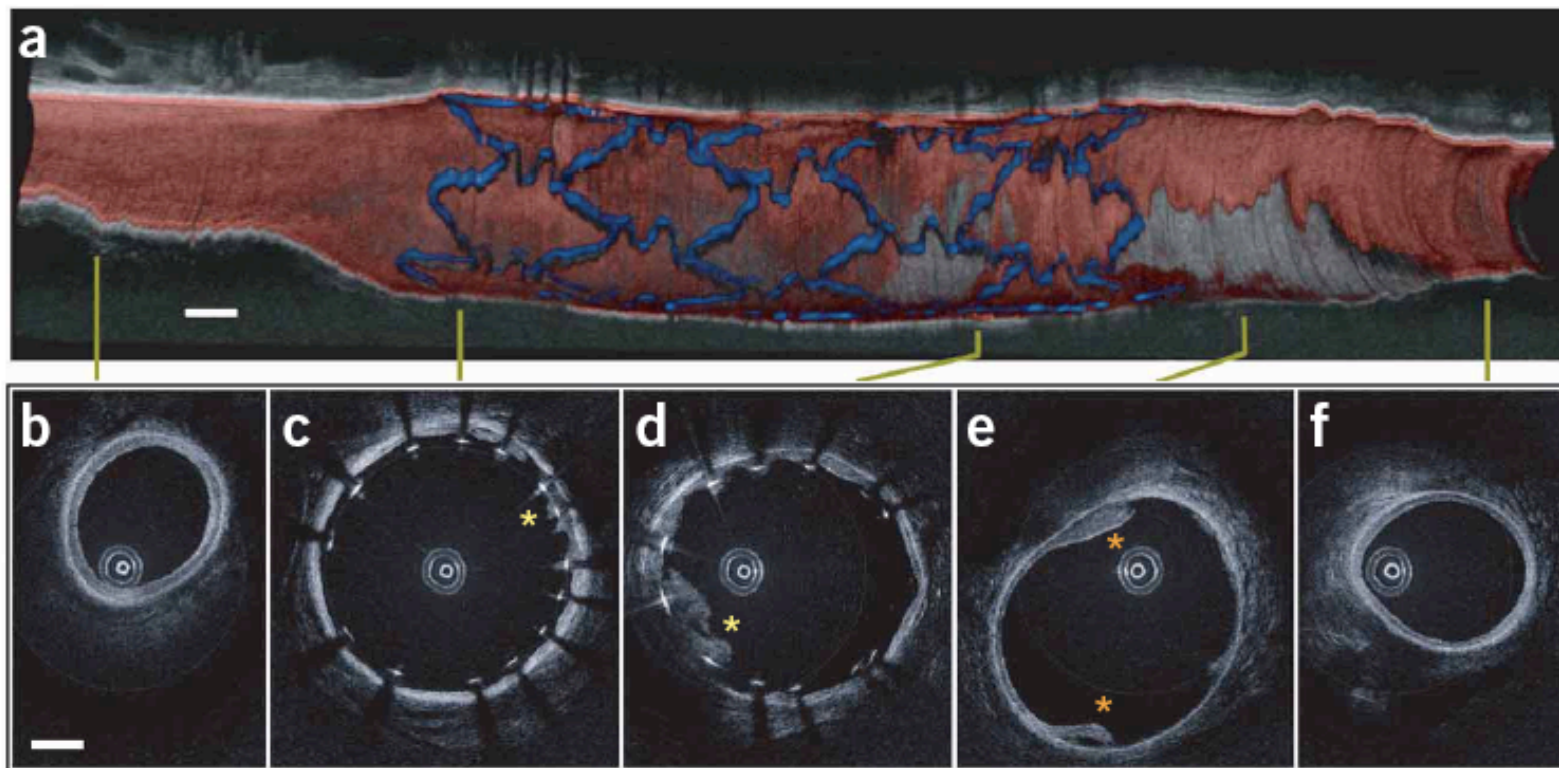


Endoscopic OCT

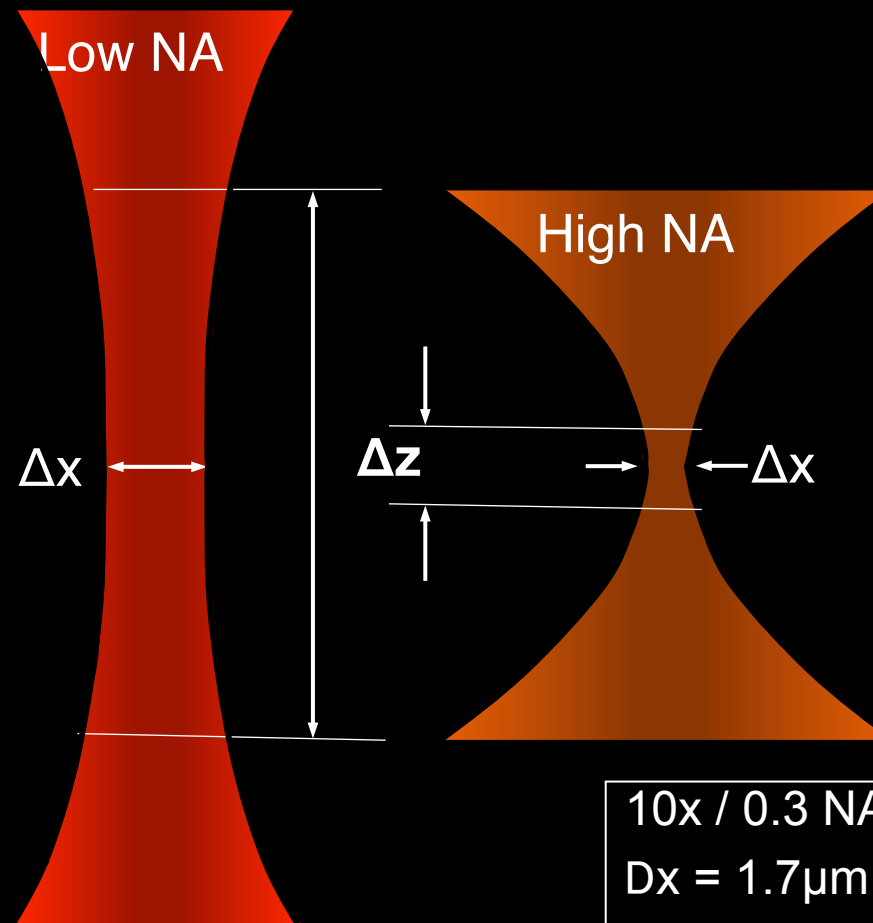


porcine coronary artery with stent in-vivo

scale bar 1mm, acquired in 6 sec



Optical Coherence Microscopy OCM



10x / 0.3 NA / 800nm

$Dx = 1.7\mu m$



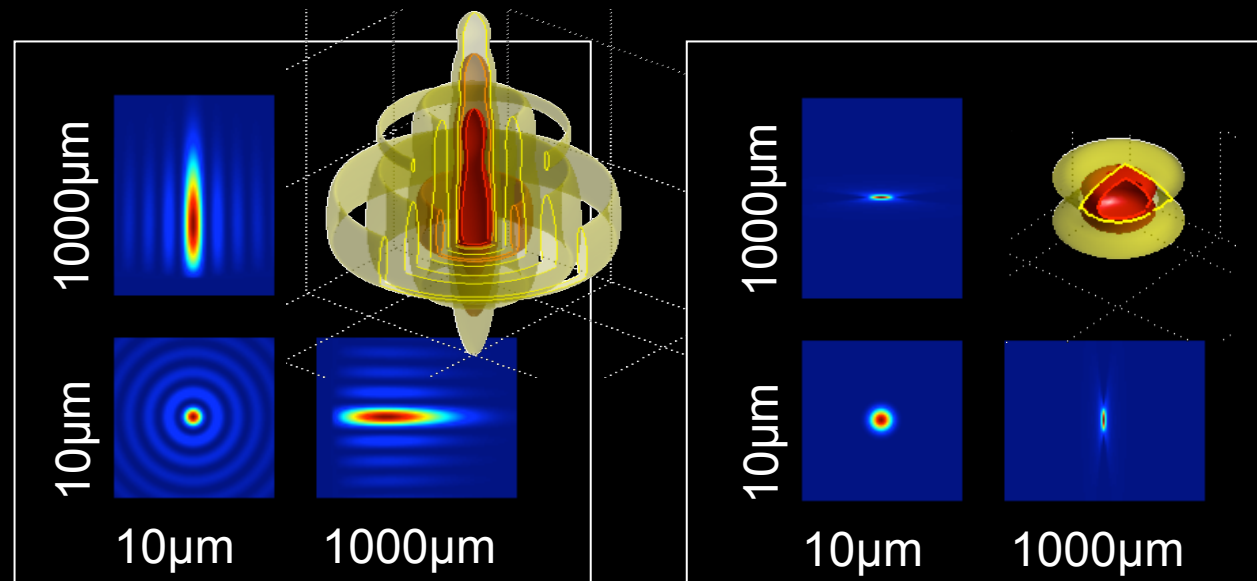
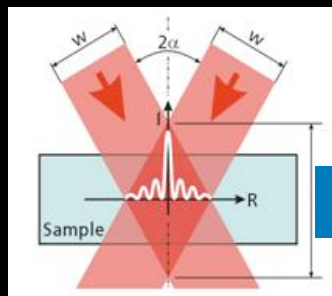
$Dz = 18\mu m$



Optical needle



Achieving a **long illumination needle** by creating an **interference pattern** in the **sample space**



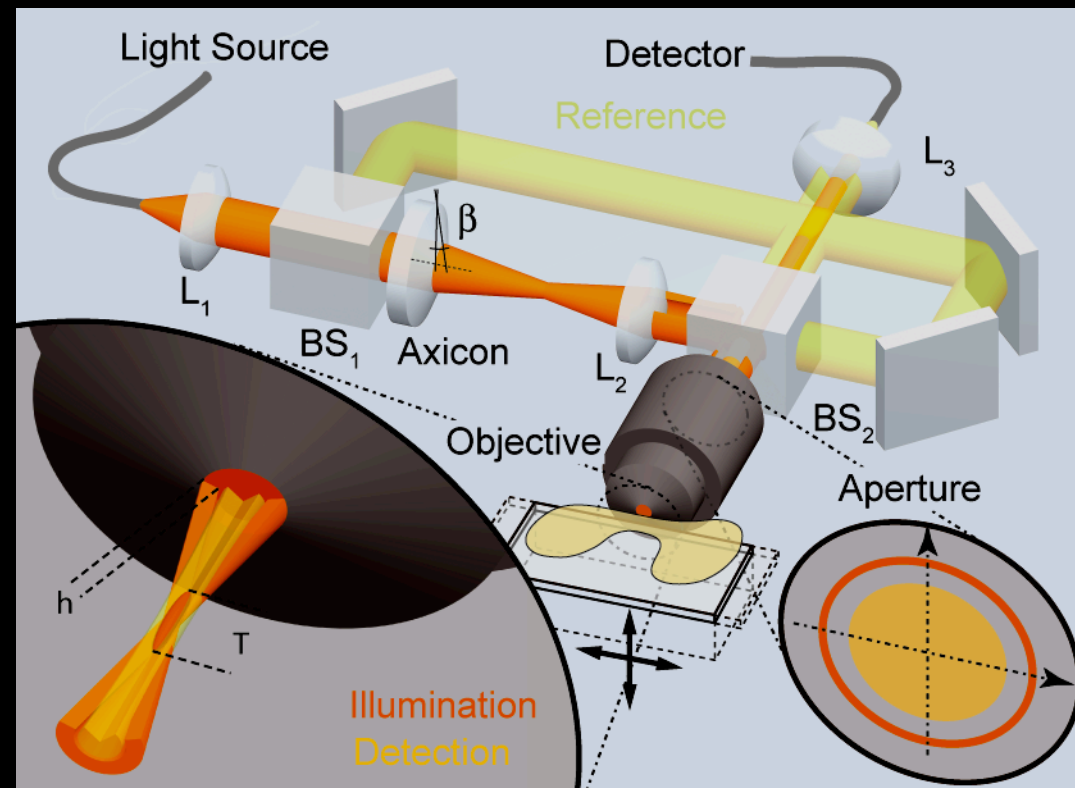
Leitgeb et al, Opt. Lett 2006

R.A.Leitgeb

Optical needle



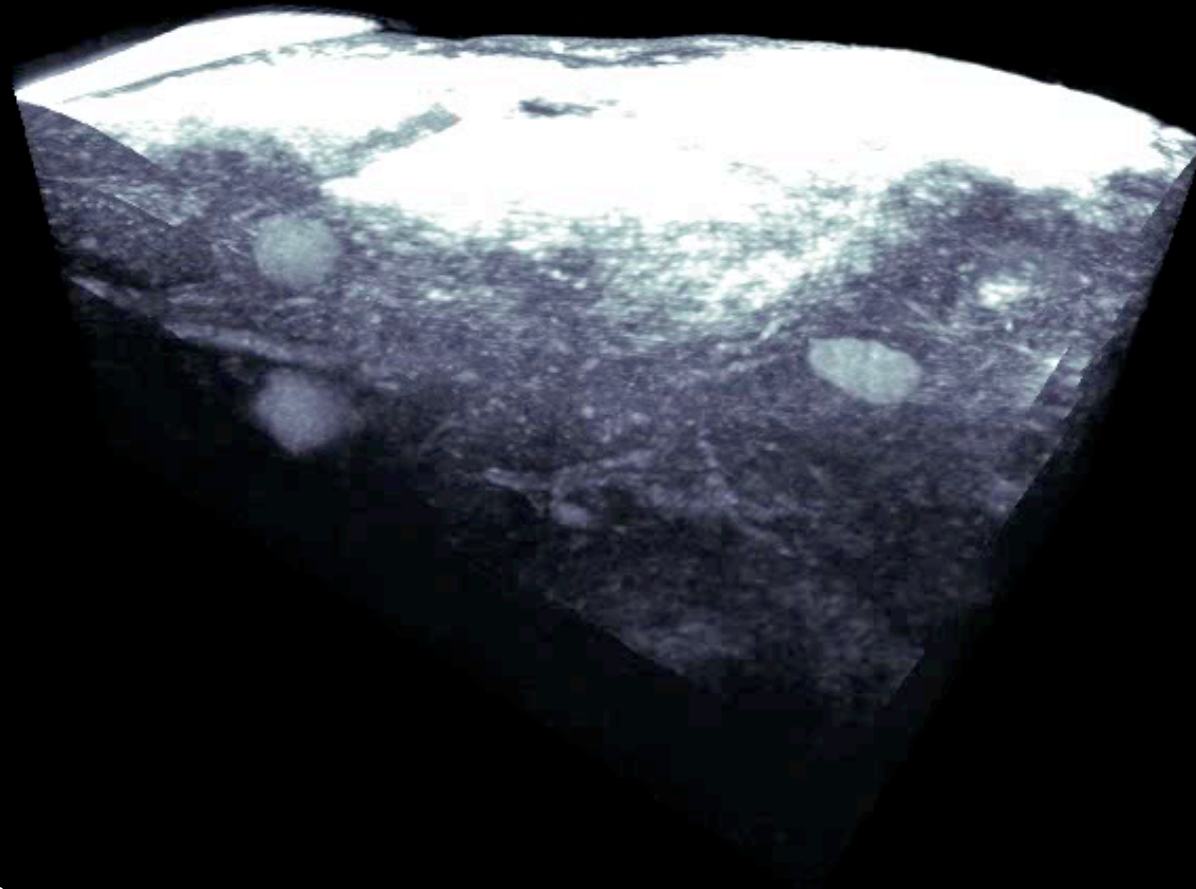
Achieving a **long illumination needle** by creating an **interference pattern** in the **sample space**



Applications – Pancreas Imaging



Application to diabetes research (visualization of Langerhans islets within unprepared mouse pancreas in-vitro and in-vivo)



2 x 1.5 mm

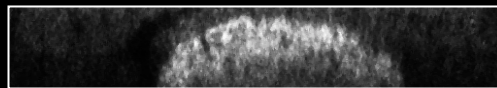
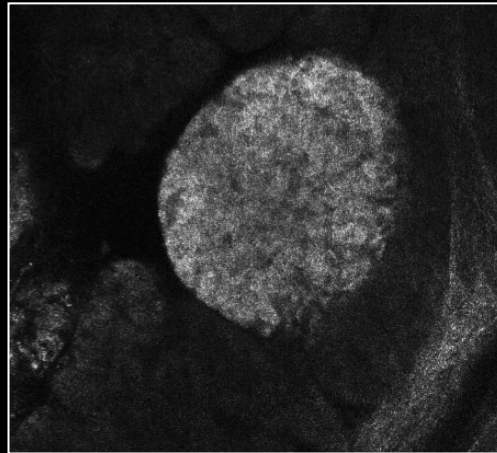
Comparison xf-OCM - confocal Microscopy



Mouse Pancreas, in vitro

400 μ m

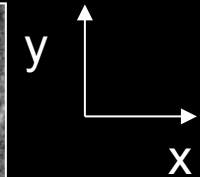
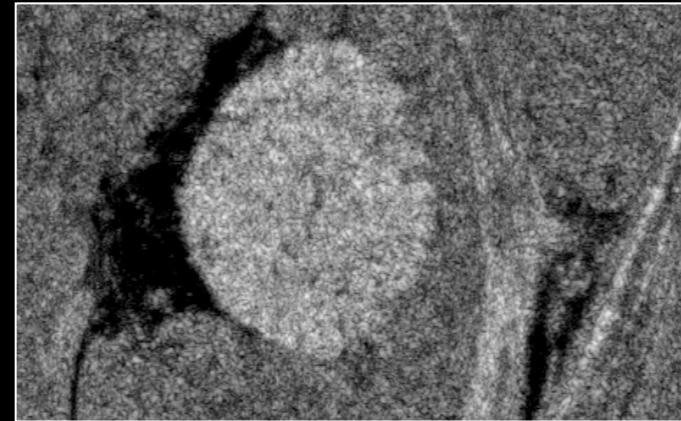
90 μ m



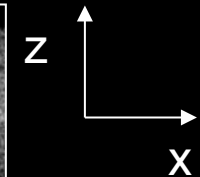
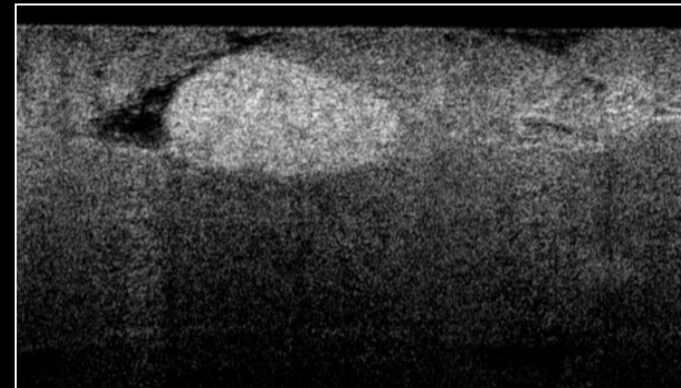
Confocal microscopy

NA 0.8, 20x water
immersion

@633nm



250 μ m



500 μ m

xf-OCM

NA 0.23, 10x air objective

@800nm

Combination xf-FDOCM-Fluorescence - Rat Hair Follicle

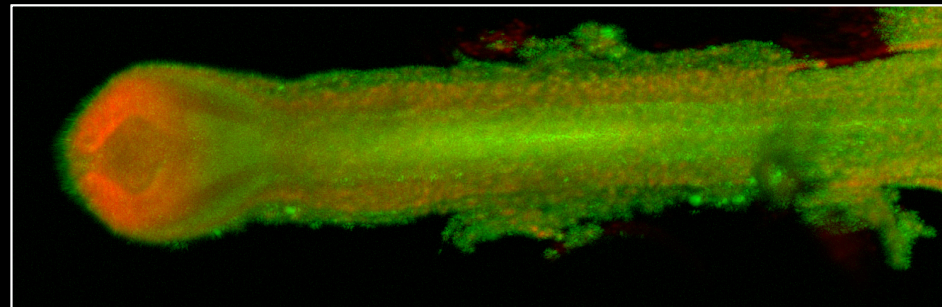


Collaboration with stem cell laboratory, EPFL : lineage
specification and cell differentiation

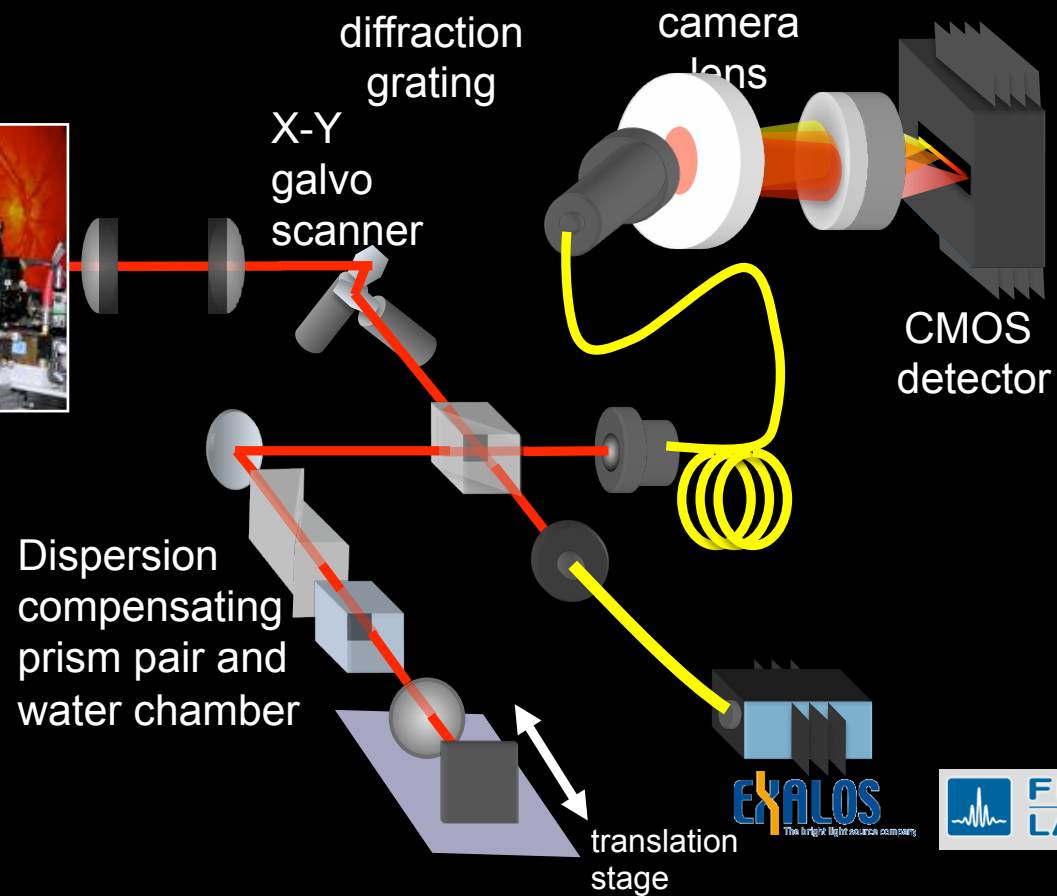


400um x 1.2mm

xf-OCM / FLM
@800nm
& 650nm



Ultra-high Speed FDOCT



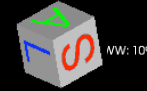
λ	830 nm
$\Delta\lambda$	45 nm
Axial resolution	6.7 μm
Line rate	up to 200 kHz
Sensitivity	92dB -103dB
Sensitivity decay	-9 dB / 2 mm
Power @ cornea	550 μW

Ultra-high Speed FDOCT



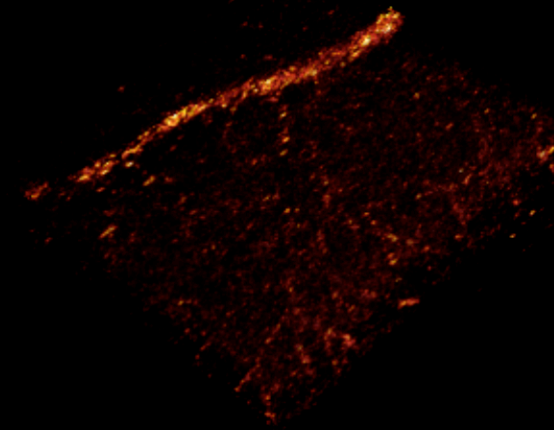
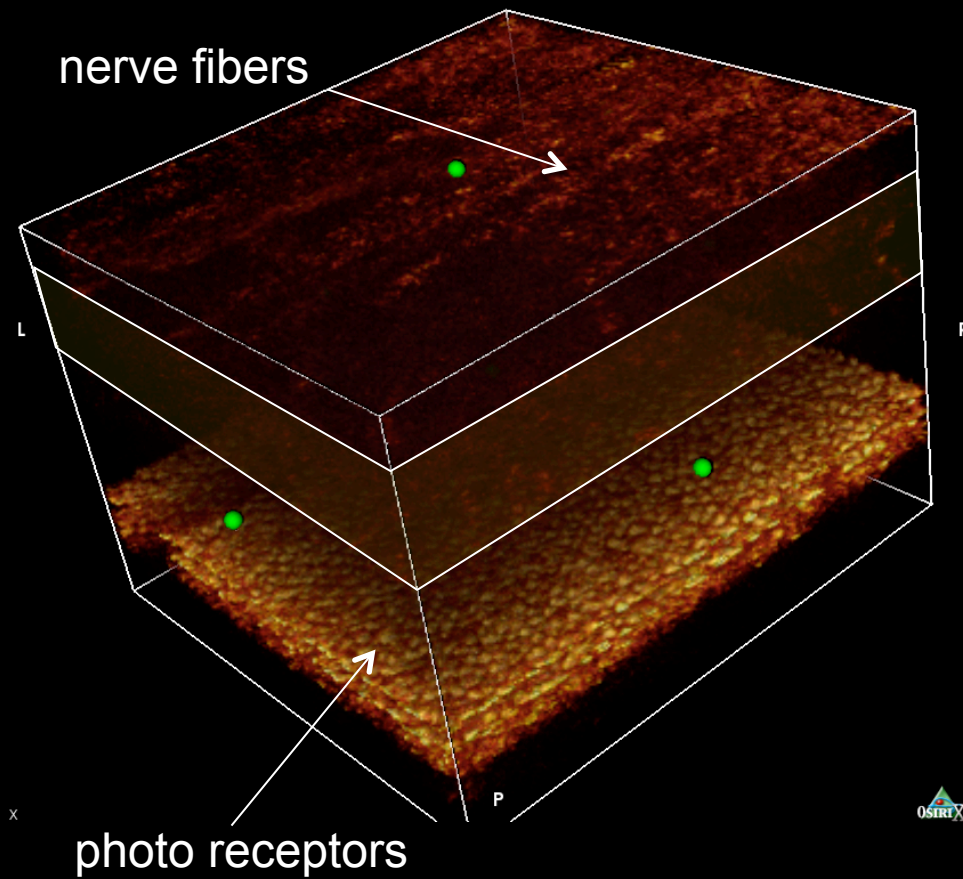
300 x 400 x 600 μm (200 x 500 x 600 pixels) taken in only 0.5sec
at 200.000 depth scans / sec

WL: 142 nm W: 200



WW: 109

A



S

P

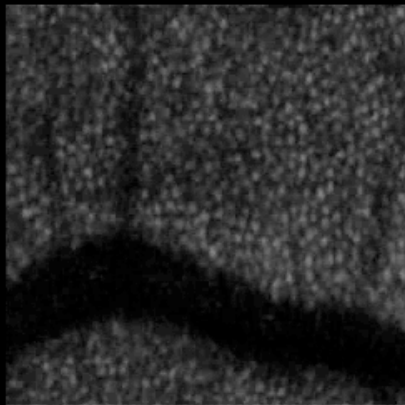


Photoreceptor Imaging without adaptive Optics

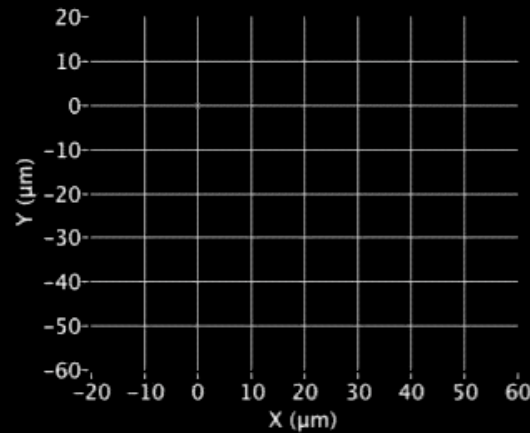


CMOS camera at 200kHz
10 full volumes per second (200x 100 x 800)
300 μ m x 300 μ m patch

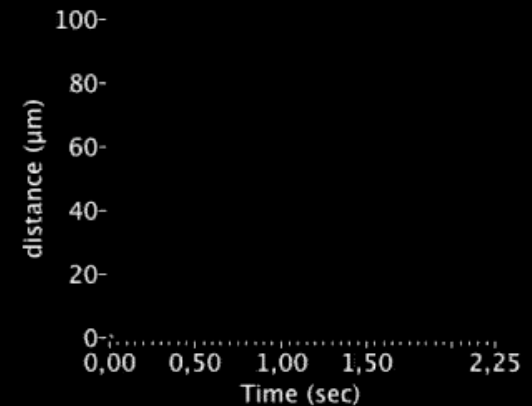
0.00 sec



Fundus projection



X-Y course of eye motion



eye motion distance

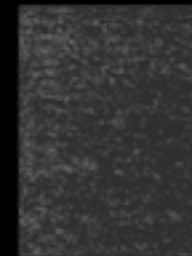
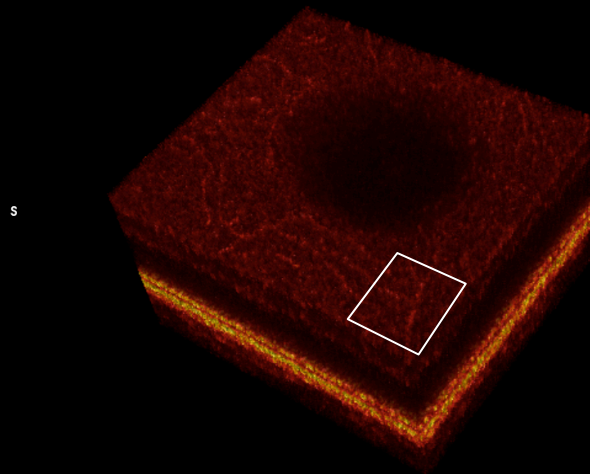
Perfusion Imaging



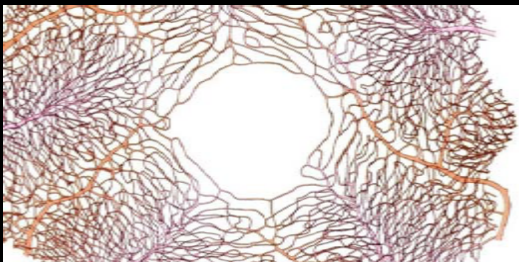
600 x 600 x 600 μm (200 x 500 x 600 pixels) taken in only 0.5sec
at 200.000 depth scans / sec



Volume series taken at
13 volumes / sec



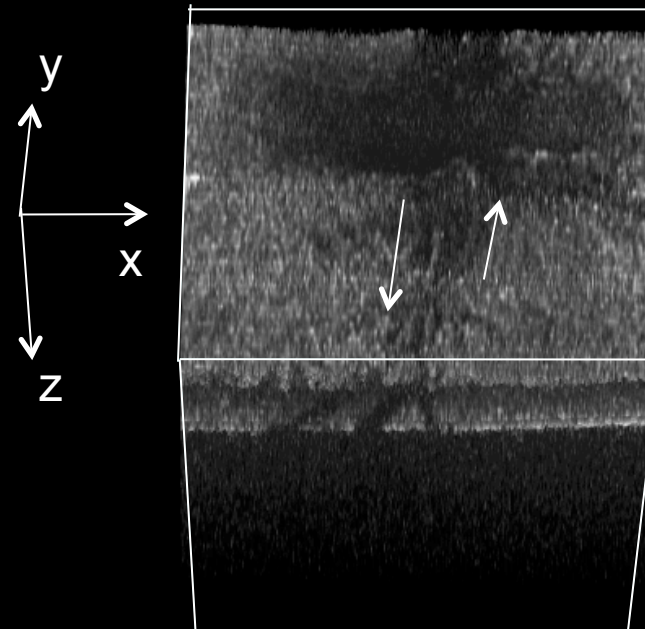
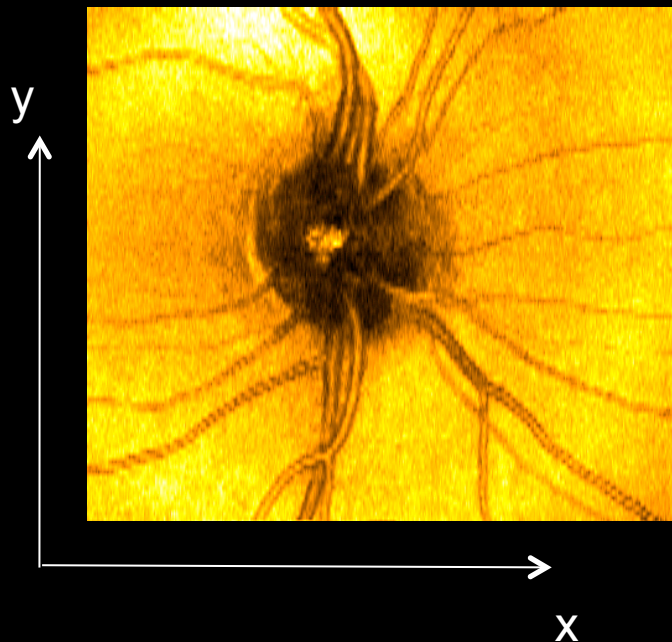
x foveal microcirculation



Perfusion Imaging



Volume series taken at
13 volumes / sec

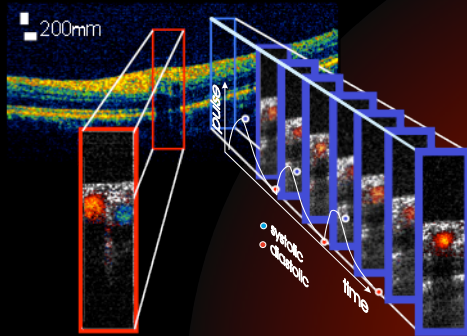


Selection of Perfusion Imaging and Contrasting Methods



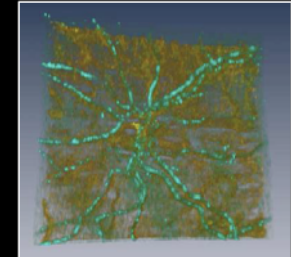
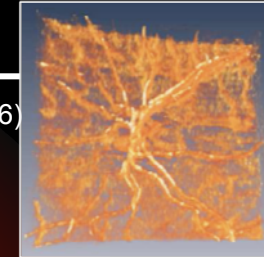
Phase sensitive –

Leitgeb et al., Opt. Express (2003)



Optical Angiography –

Makita et al., Opt. Express 14 (2006)

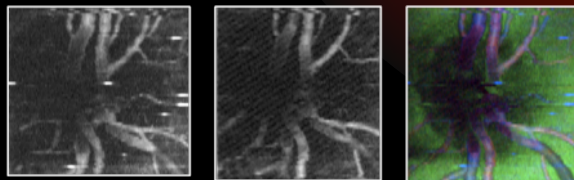


Perfusion Imaging with OCT

Joint time and frequency domain Doppler –

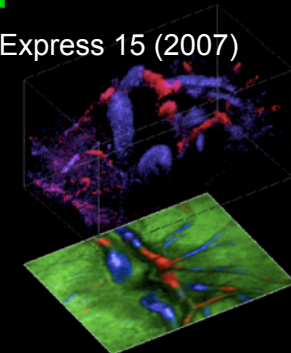
Szkulmowski et al, Opt. Express 16 (2008),

Tao et al. Opt. Express 16 (2008)



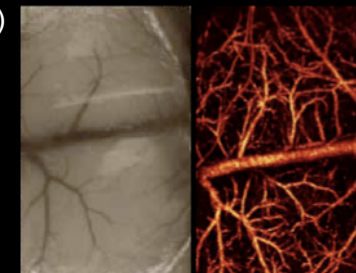
Resonant Doppler –

Bachmann et al., Opt. Express 15 (2007)



Optical Micro-Angiography (OMAG) –

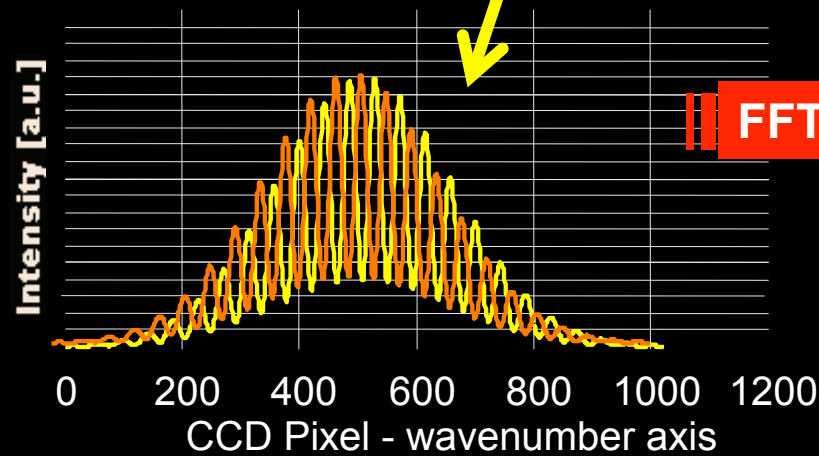
Wang et al. Opt. Express 15 (2007)



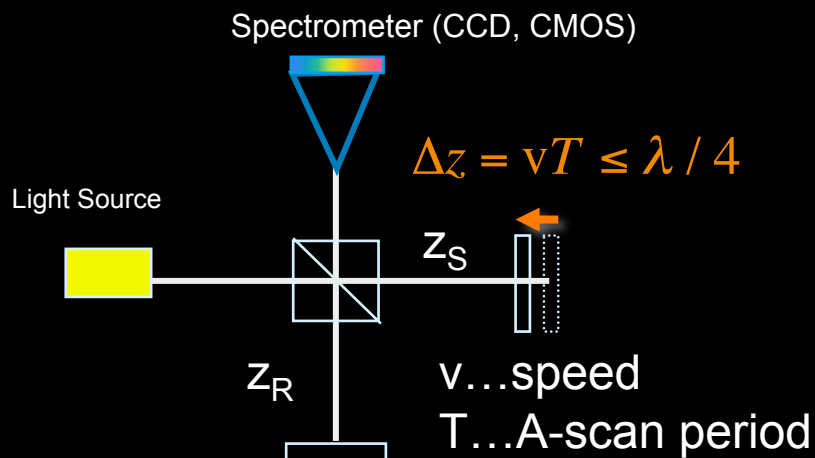
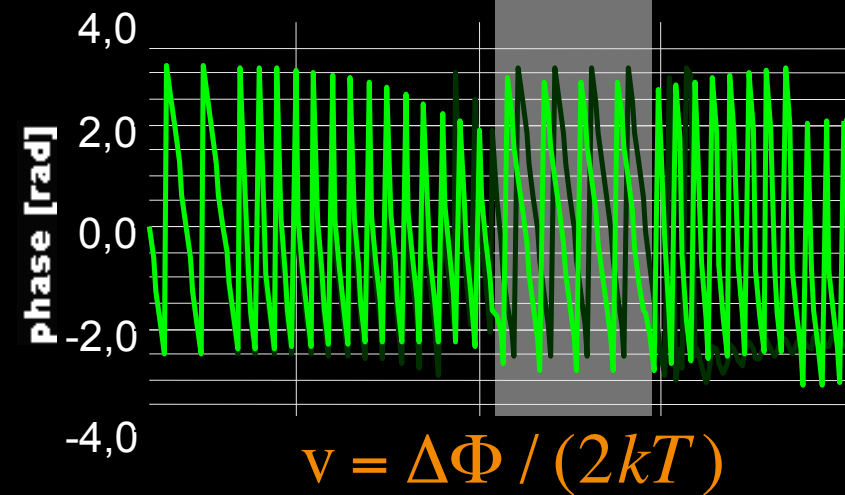
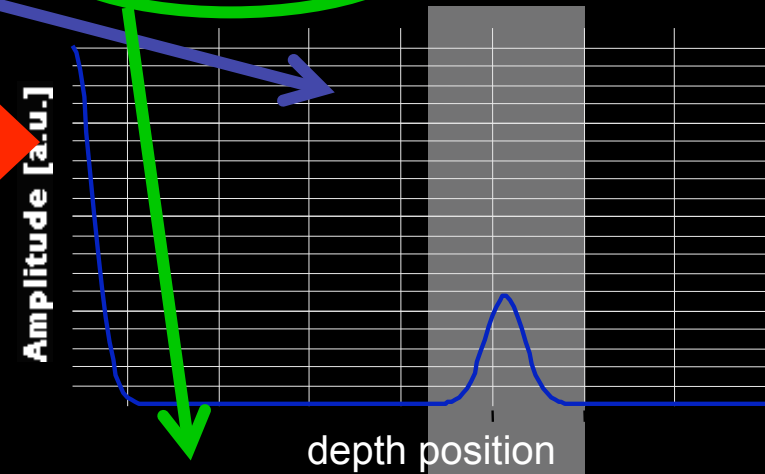
Method - Doppler FDOCT



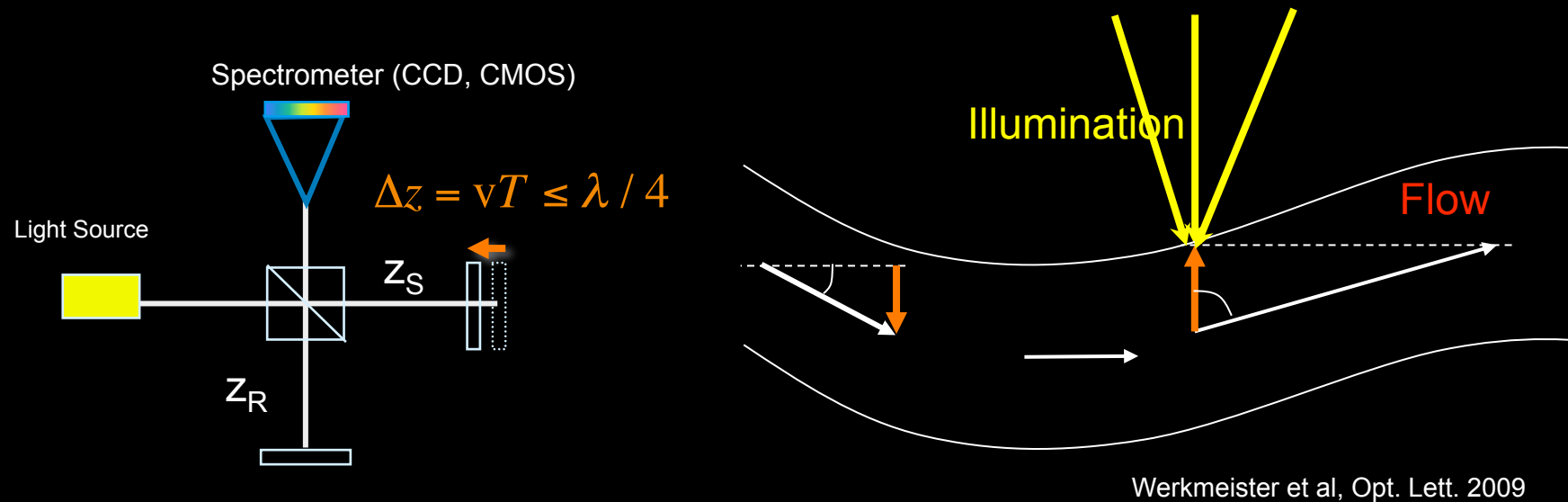
$$FFT \{ I(k) \} = \hat{I}(z) \exp(i\Phi(z) + 2ikvT)$$



FFT



Method - Doppler FDOCT



Within order $10\mu s$ typical exposure time of CCD retinal blood moved only 10nm !!!

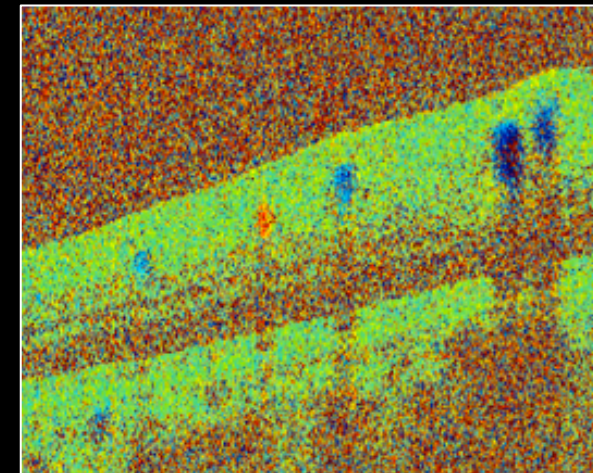
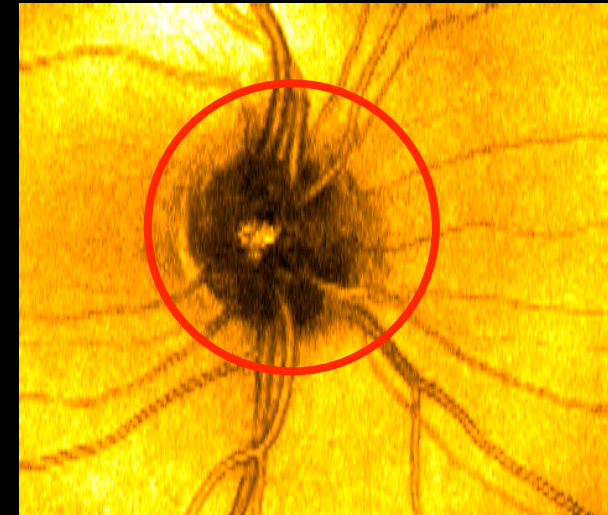
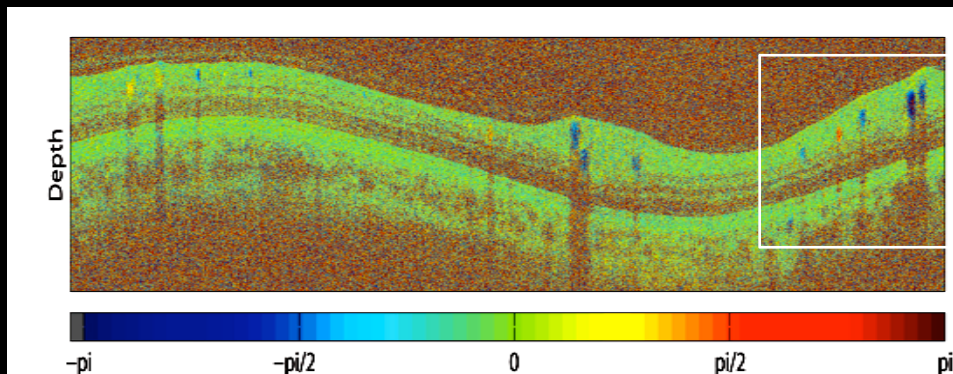
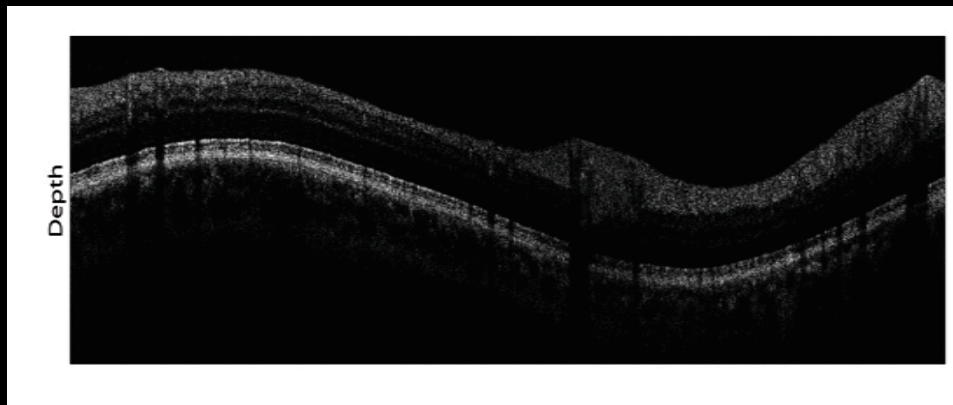
Like looking at lake Geneva from airplane and detect height changes corresponding to thickness of a single hair.

Method - Doppler FDOCT

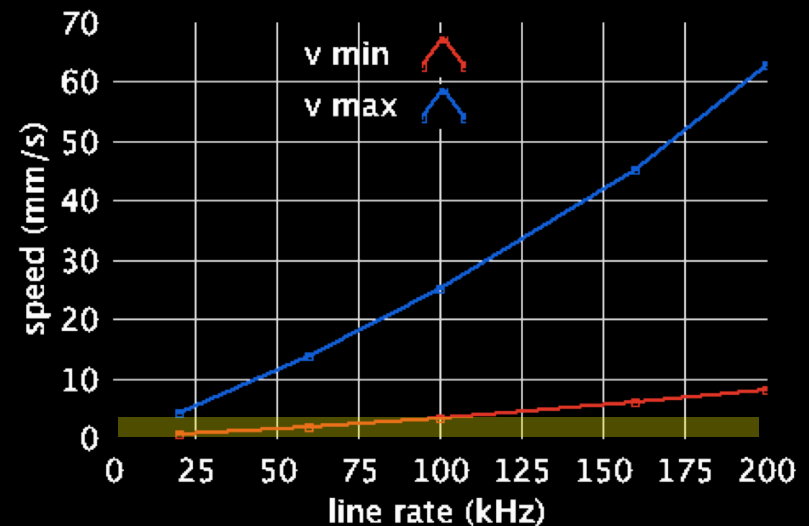
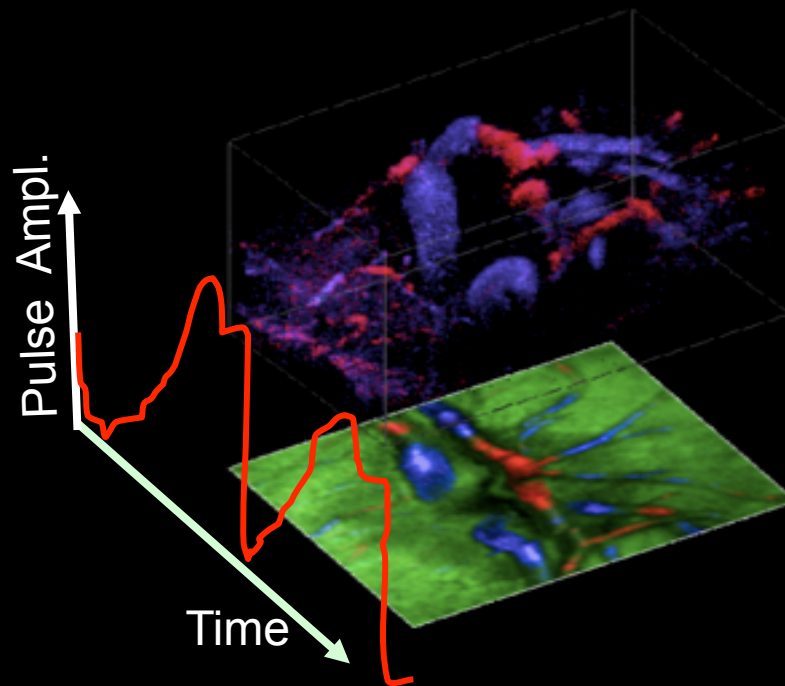


Circumpapillary scans

8000 A-scans, 30kHz scan rate



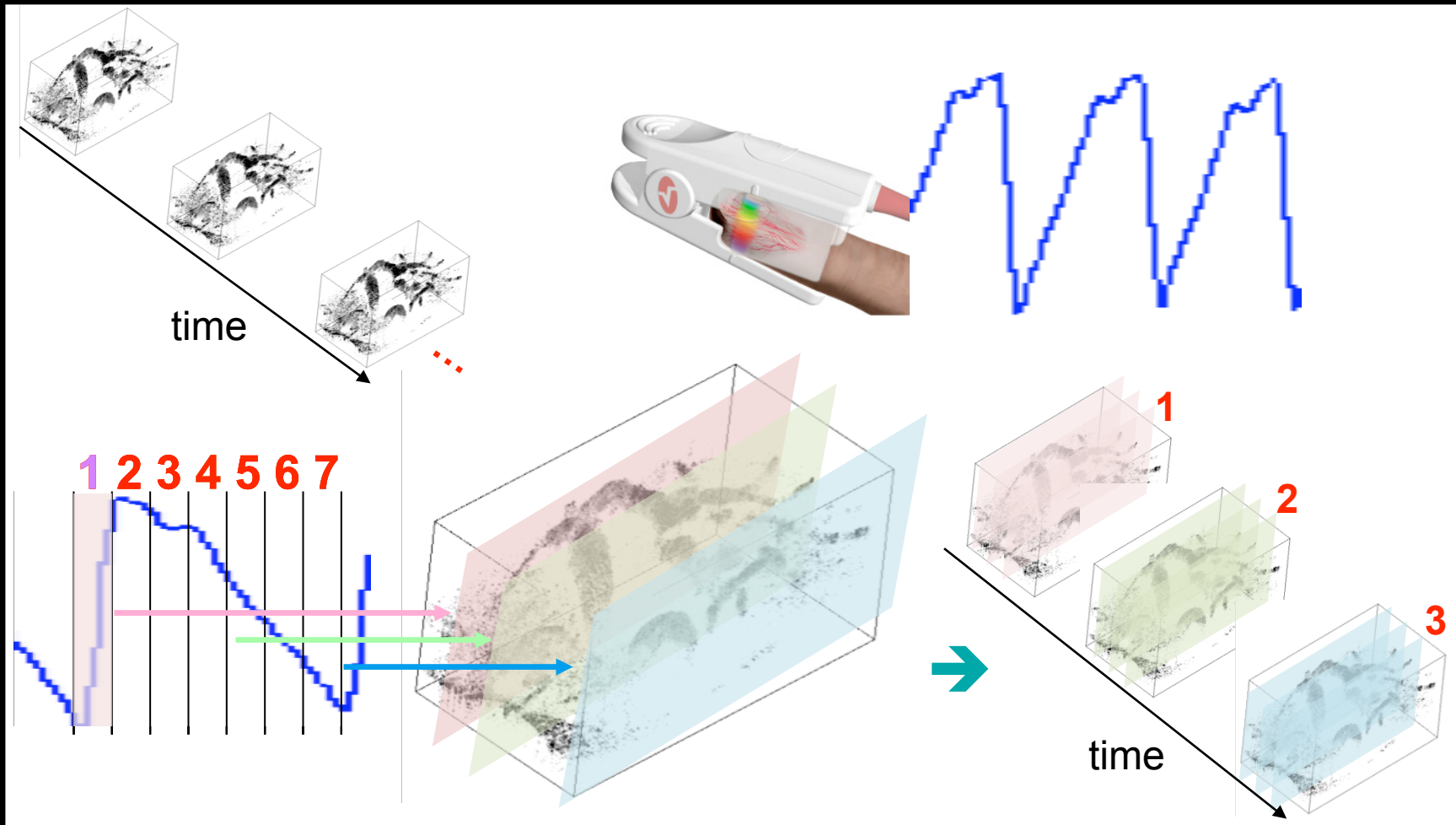
Pulse Coherent 4D Angiography



Acquisition time for a volume with sufficient sampling for quantitative analysis spans over several heart cycles.

➔ **difficult to observe quantitative retinal perfusion heartbeat phase coherently in 4D**

Cyclic Reconstruction of 4D Retinal Blood Flow

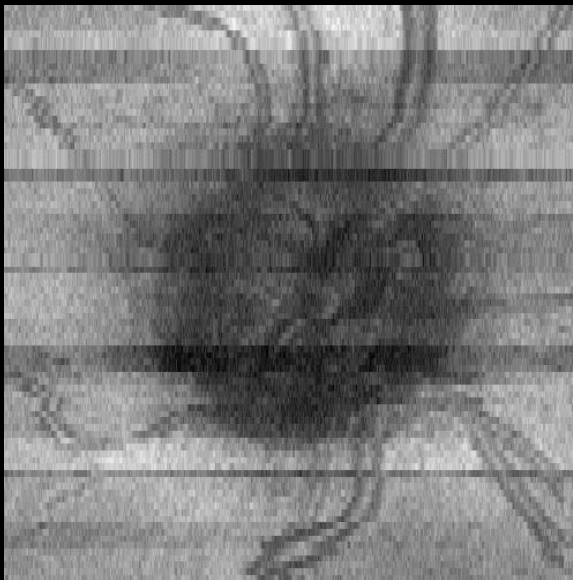


Results

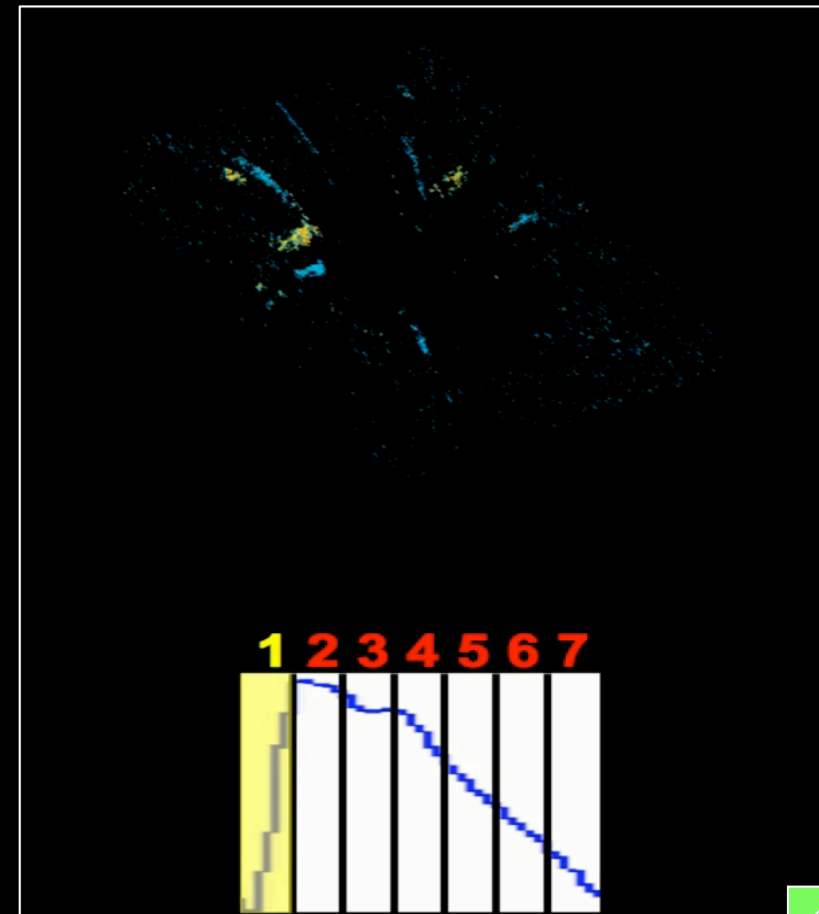


Z-projections of 7 recombined phase coherent volumes:

OCT – fundus view



4D-pulse coherent Doppler - OCT



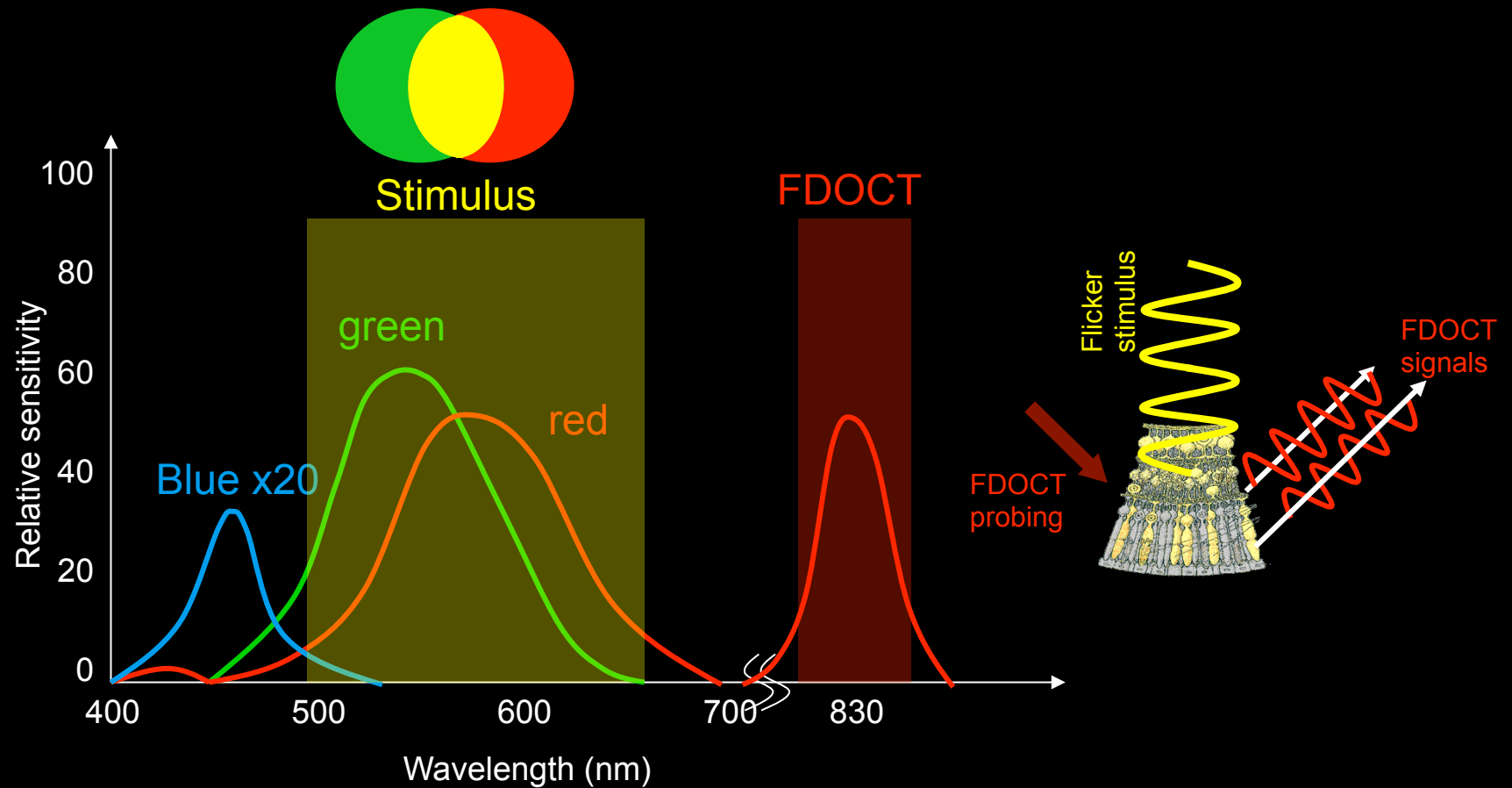
Motivation for optical Assessment of Neural Tissue Responses



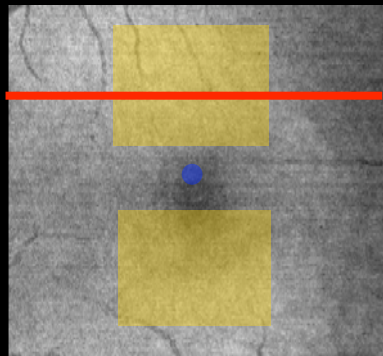
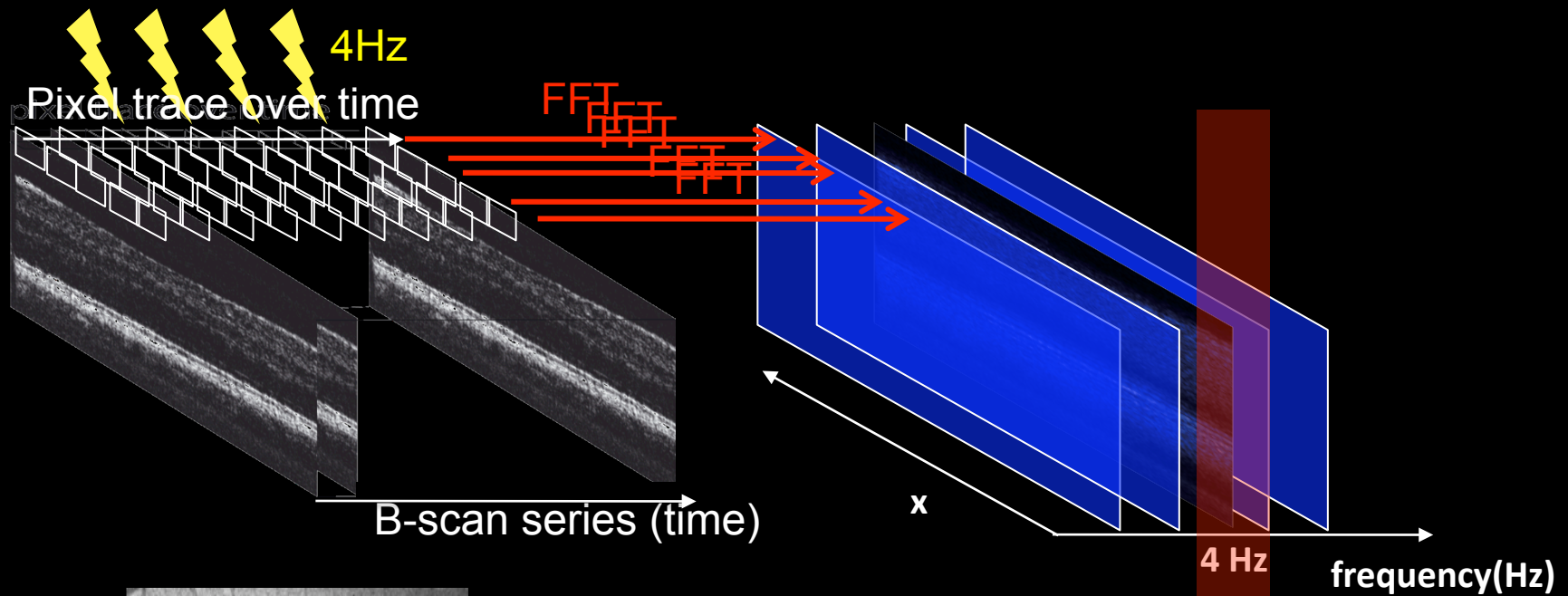
Availability of Techniques to assess signaling pathways and photoreceptor functionality in-vivo are limited.

Optical methods that detect changes in retinal reflectivity as a response to flash stimuli indicate a direction for **probing of retinal functionality depth resolved in a completely non-invasive way**

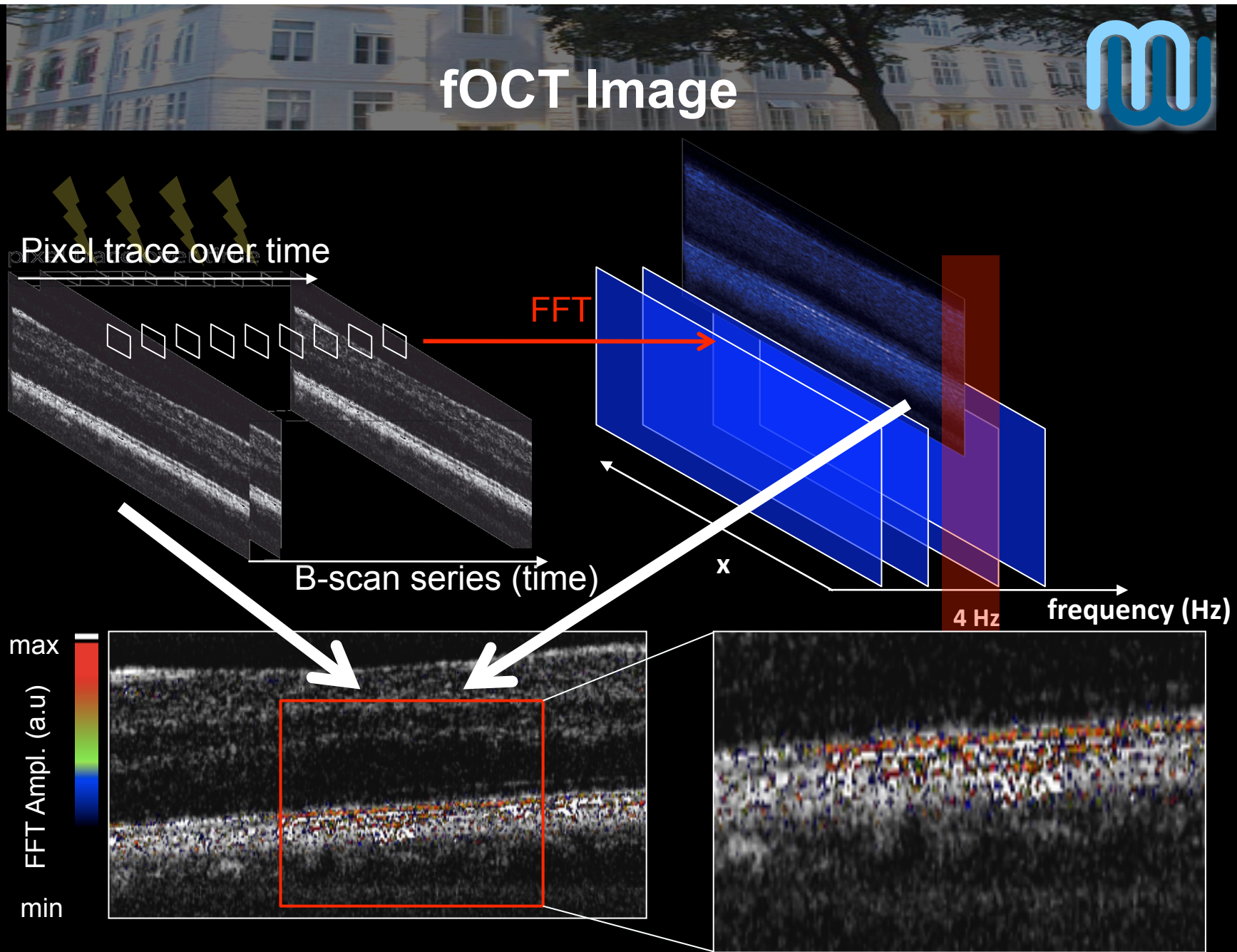
Stimulus / Probing Spectra



Data Processing



B-scan series at 60Hz (13ms / sample)
1000 scans/ B-scan at 60kHz (CMOS)
Flicker at 4Hz
30 μ W stimulus intensity at cornea
60 μ m spot size on the retina
B-scan series is registered prior to FFT !





Conclusion

- OCT does not only provide excellent resolution and high sensitivity it also profits from functional extensions that make use of the richness of information light carries.
- Novel light source and detector technology enable dynamic volumetric imaging opening new perspectives to understand tissue physiology and patho-physiology
- Novel developments will also focus on the delivery of OCT probing light to internal organs and in particular to the vascular system.
- Will OCT gain in molecular specificity ? Perhaps in combination with other techniques such as multi-photon microscopy.



Acknowledgments

PhD Students: Adrian Bachmann, Roland Michaely, Martin Villiger, Tilman Schmoll

Diploma Students: L. Steinmann, C. Imboden, C. Blatter, C. Pache,
E. Seise, C. Rödel, R. Vuillamy, Christoph Kolbitsch

Coherent Imaging Team, Colleagues at LOB, EPFL

C. Vélez, EXALOS AG, Switzerland

FEMTOLASERS, Inc, Vienna, Austria

Swiss Collaborators: Theo Lasser (EPFL), Cathrin Briskin (ISREC), Paolo Meda (HUG)

Swiss National Fonds FNS 205321-109704/1, Swiss SATW Grant, TK-06-01
FP7 –EU project FUN-OCT



Thank you for your attention...

rainer.leitgeb@meduniwien.ac.at

R.A.Leitgeb