

# Laser-based photoacoustic sensing of glucose in aqueous samples

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3<sup>rd</sup> of November 2010 Bern



# Outline

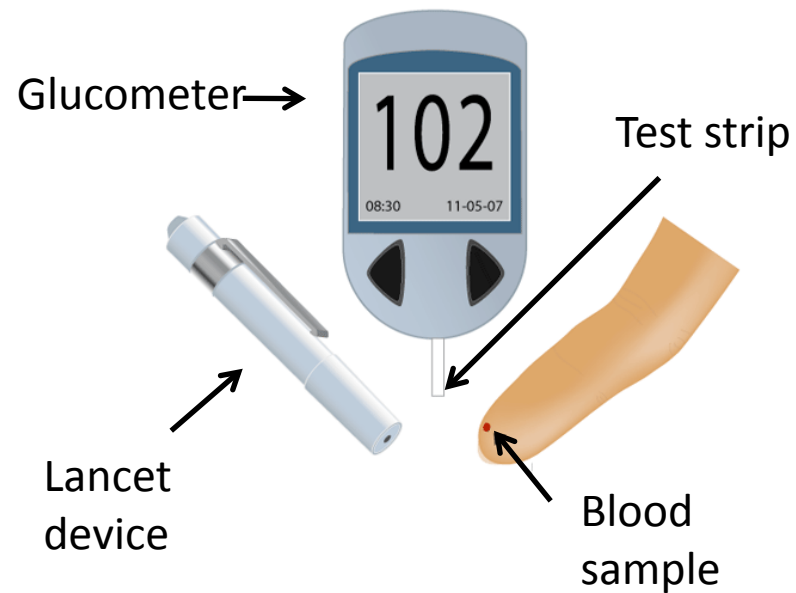
- Motivation
- Experimental Technique and Setup
- Results
- Conclusion and Outlook



# Motivation

Diabetes as a human metabolic disease:

- Patients need to measure their blood sugar level several times per day
- Preprandial glucose level of a healthy human: 65 – 120 mg/dl
- Common blood sugar measurements are invasive



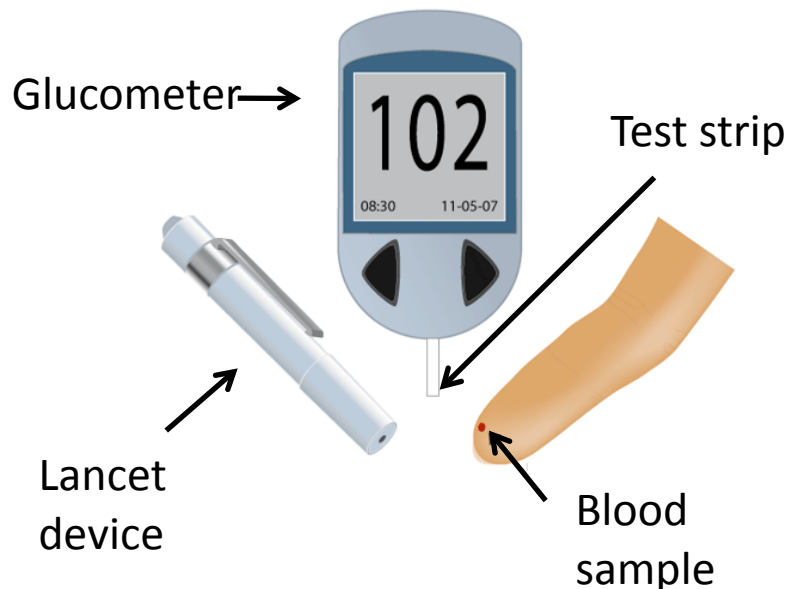
# Motivation

Diabetes as a human metabolic disease:

- Patients need to measure their blood sugar level several times per day
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**Goal:** Development of a **non-invasive** glucose sensor based on

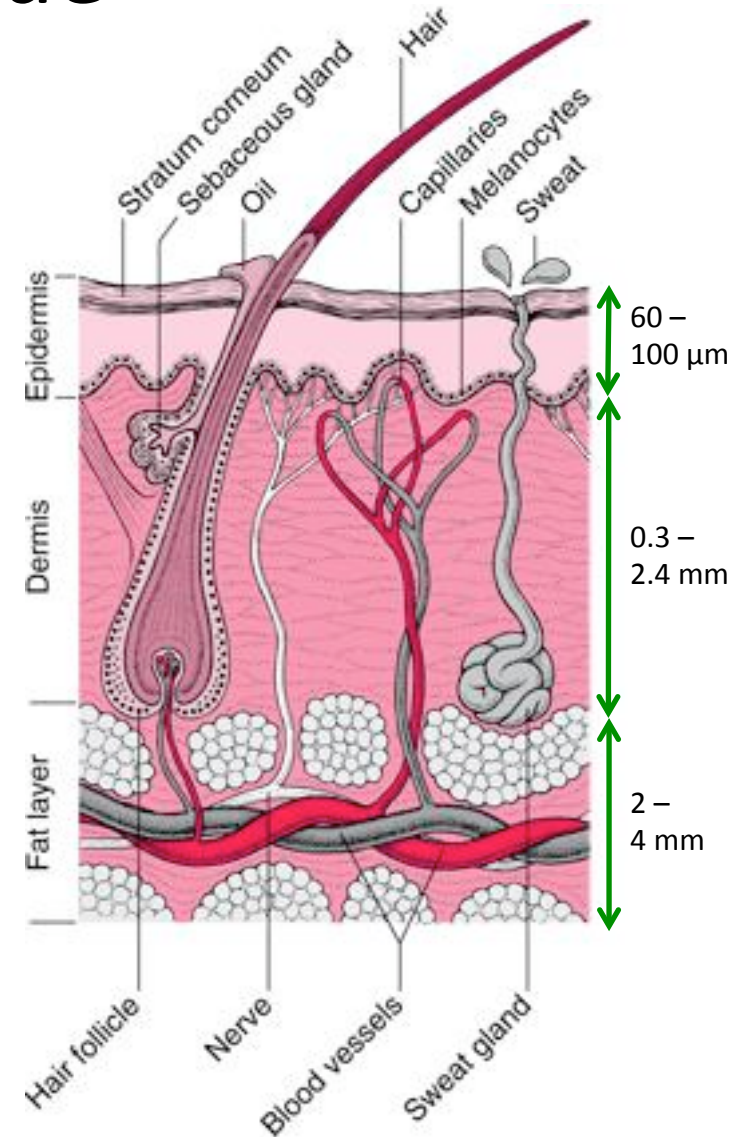
- MIR spectral region
- Photoacoustic (PA) detection
- Interstitial fluid glucose





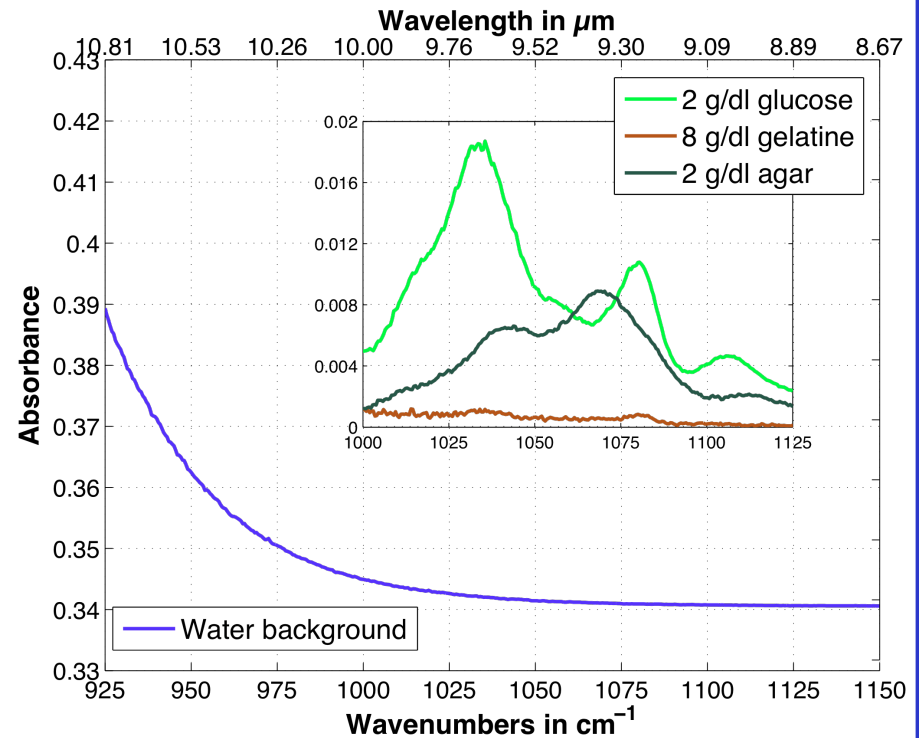
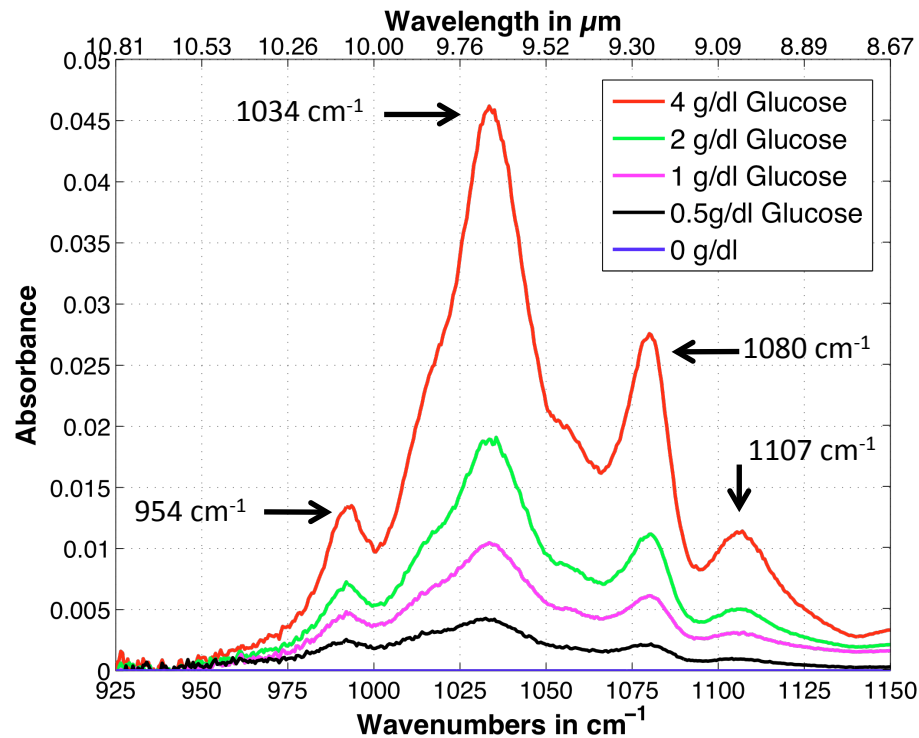
# Human tissue

- The stratum corneum is between 10-20  $\mu\text{m}$  thick with 10% water content
- Epidermis is usually between 60-100  $\mu\text{m}$  thick, has a 60% water content and is not supplied with blood
- In the MIR only up to approx. 100  $\mu\text{m}$  optical penetration depth
- Measurements of glucose concentration in the interstitial fluid (ca. 15 min time delay)



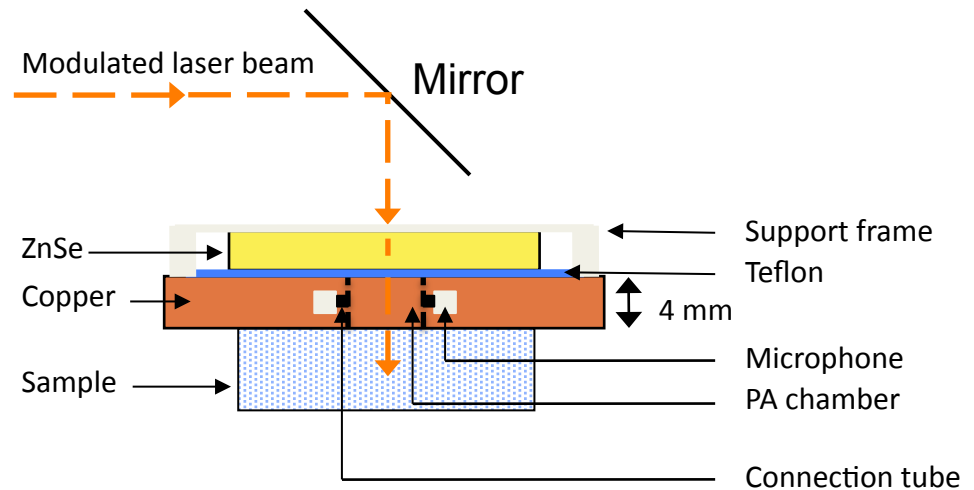
# Glucose and phantom tissue

- Water, gelatine and agar as a first step towards mimicking tissue
- Characteristic glucose absorption peaks at 1034 and 1081  $\text{cm}^{-1}$
- Strong absorption of water in the MIR



# Photoacoustic effect and cell design

- Volume 80 mm<sup>3</sup>

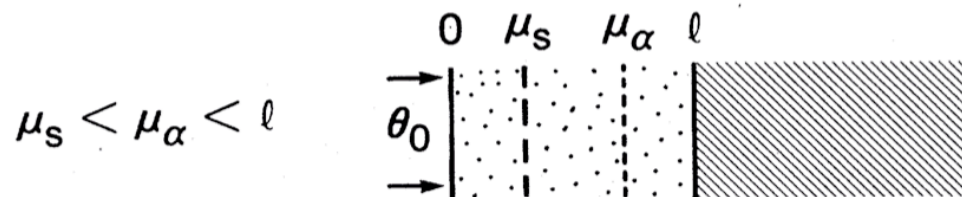


## Gas piston model:

Optically and thermally thick case

$$\text{PA signal} \propto \frac{I \cdot \alpha}{V \cdot f^{1.5}}$$

Tam C., Rev. Mod. Phys., 1986, **58**, 381-434

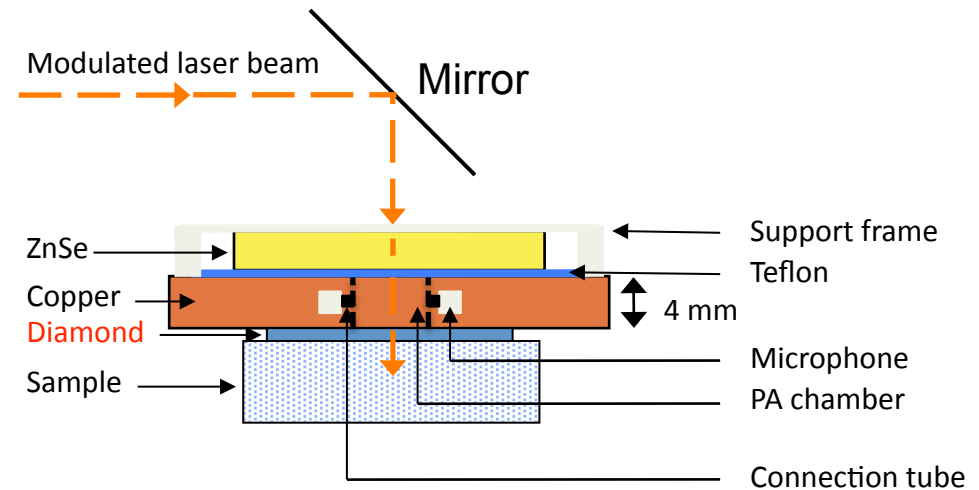


$$\mu_s = \left( \frac{D_s}{\pi f} \right)^{\frac{1}{2}} \text{ with } D_s = \text{thermal diffusivity}$$

$$\mu_a = \frac{1}{\alpha} \text{ with } \alpha = \text{absorption coefficient}$$

# Photoacoustic effect and cell design

- Volume 80 mm<sup>3</sup>
- Diamond window 163 μm

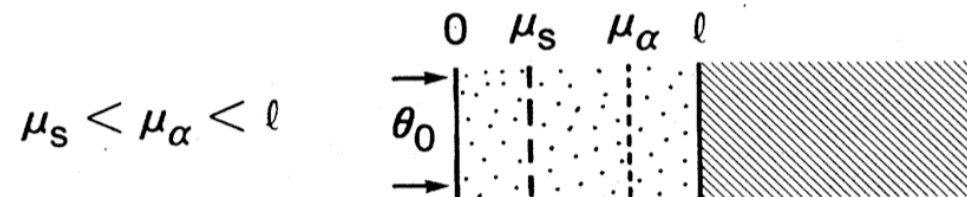


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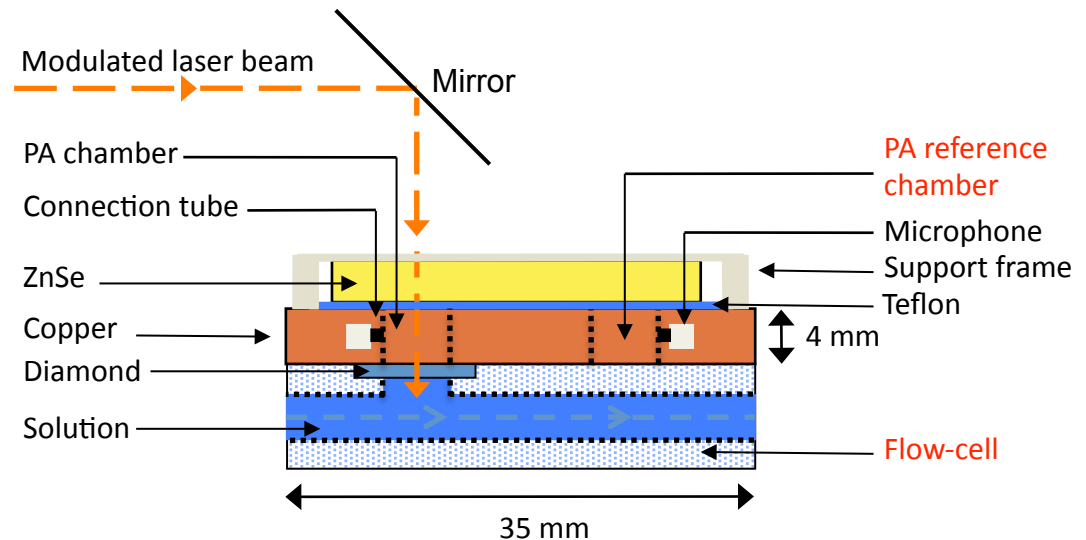
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# Photoacoustic effect and cell design

- Volume 80 mm<sup>3</sup>
- Diamond window 163 μm
- Flow cell
- Reference chamber

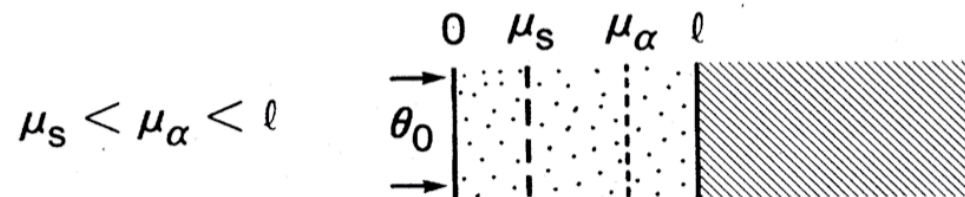


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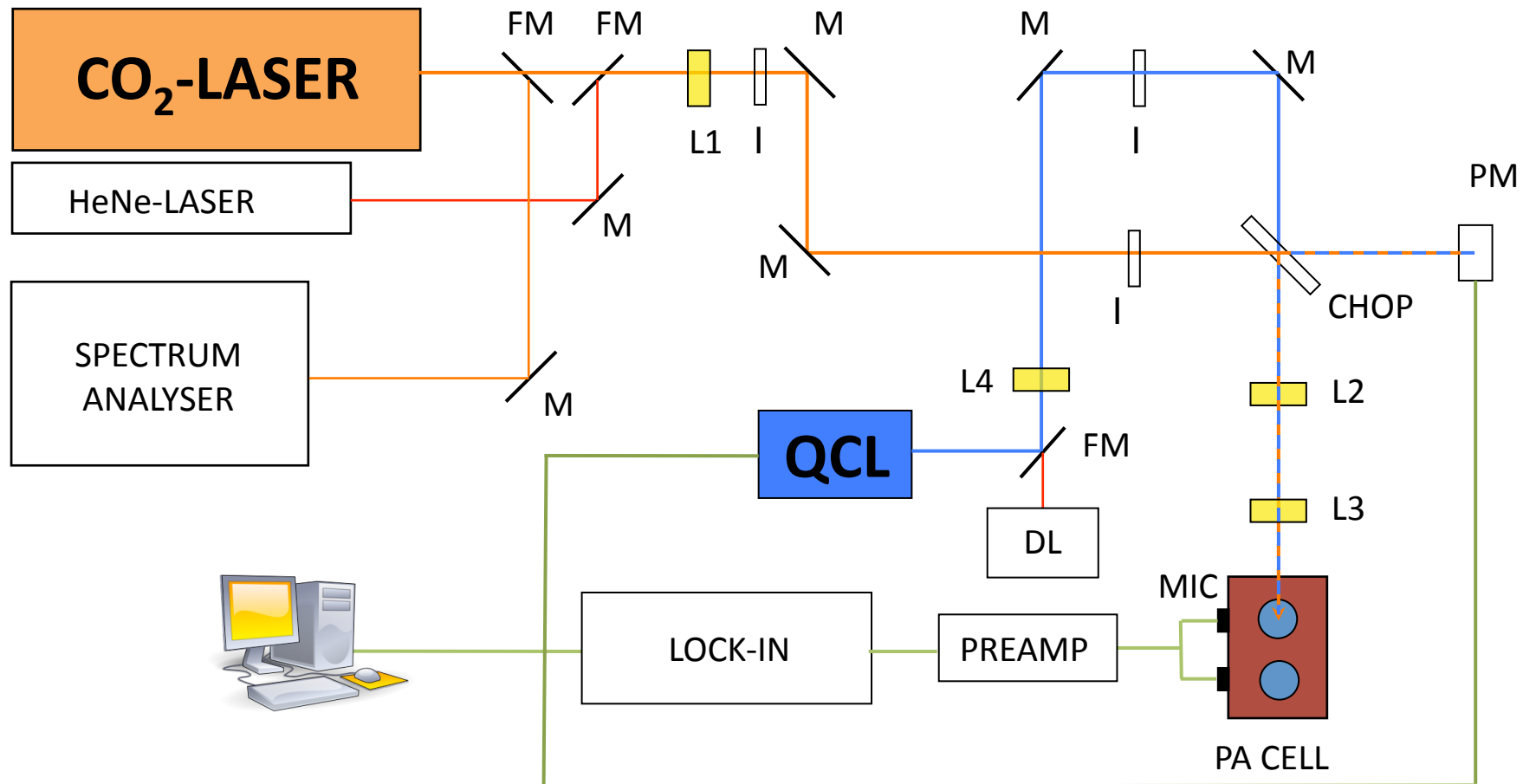
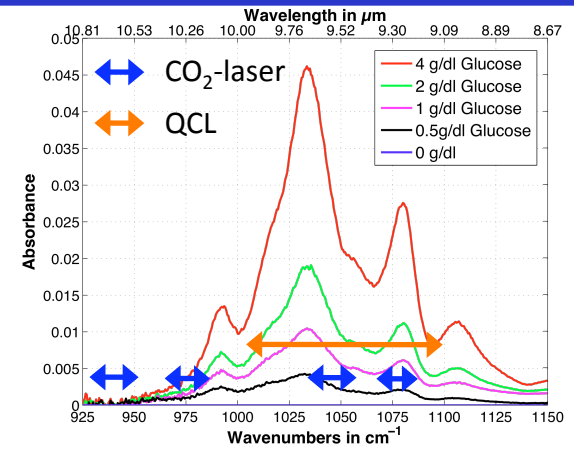
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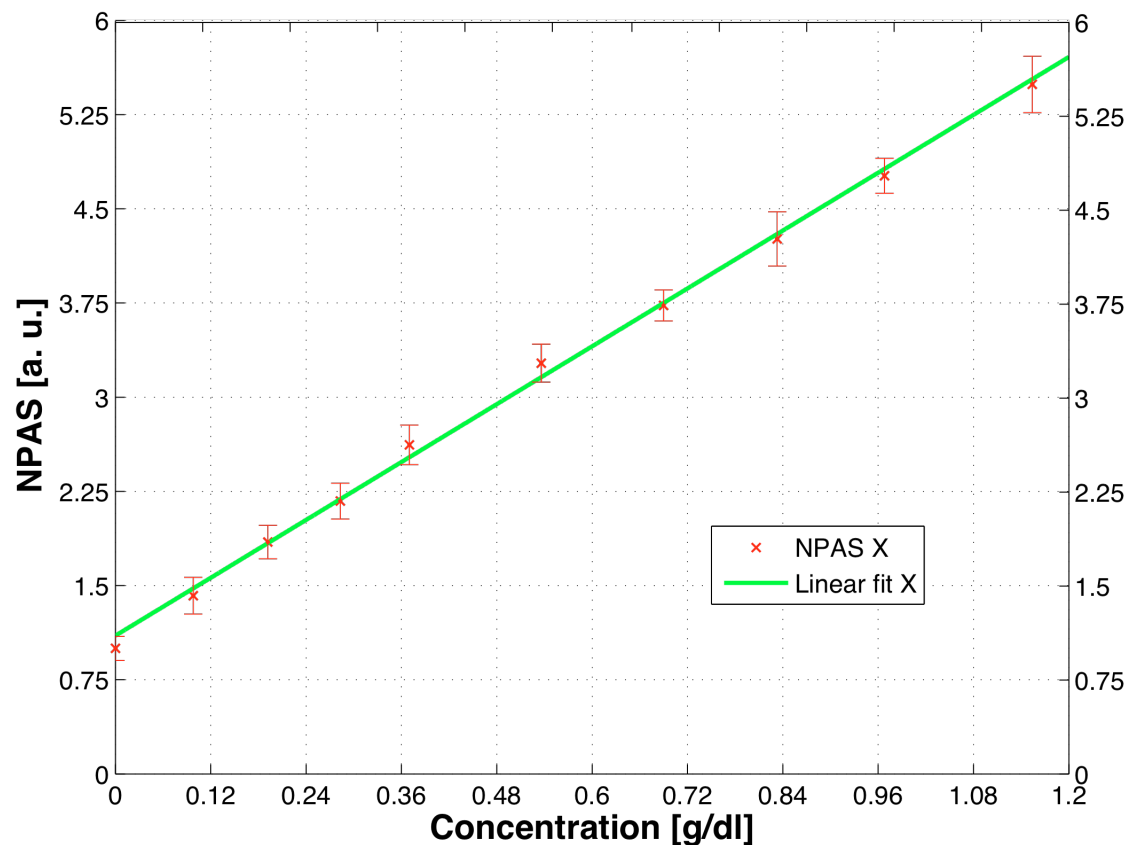
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# Experimental setup

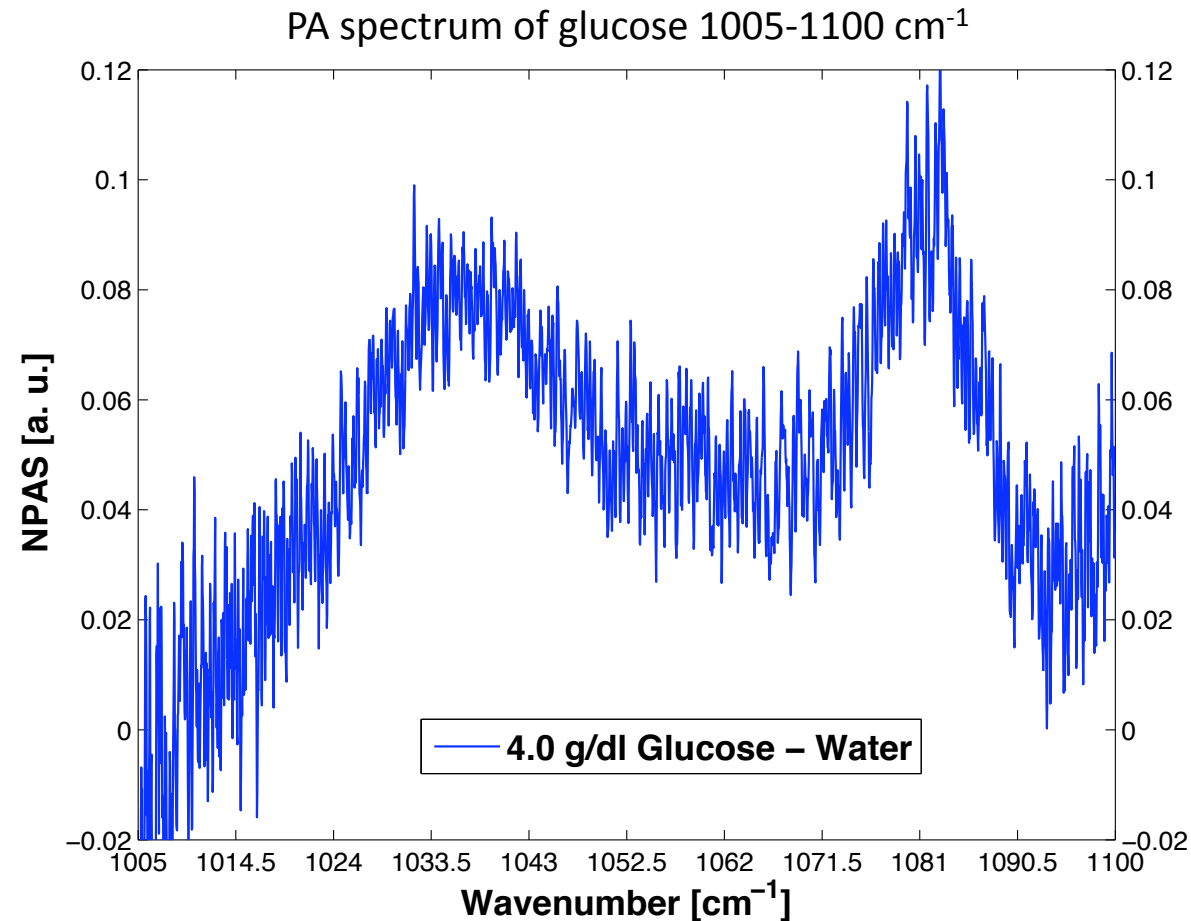


# Glucose depending NPAS measured with the flow cell



- NPAS at  $1082\text{ cm}^{-1}$  (QCL) –  $944\text{ cm}^{-1}$  ( $\text{CO}_2$ -laser) measured in PA chamber A
- NPAS reference measurement measured in chamber B (without laser)
- Shown signal A – B
- 100 mg/dl detectable

# Fast recording of a spectrum with the QCL

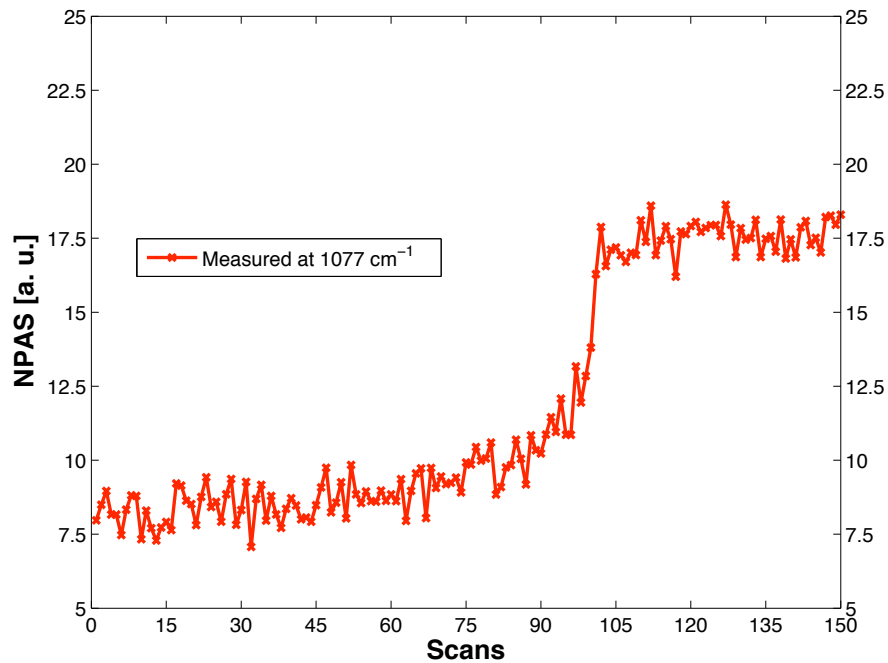


- A single spectrum can be recorded within 5.5 s
- An averaging of the single measurement is necessary



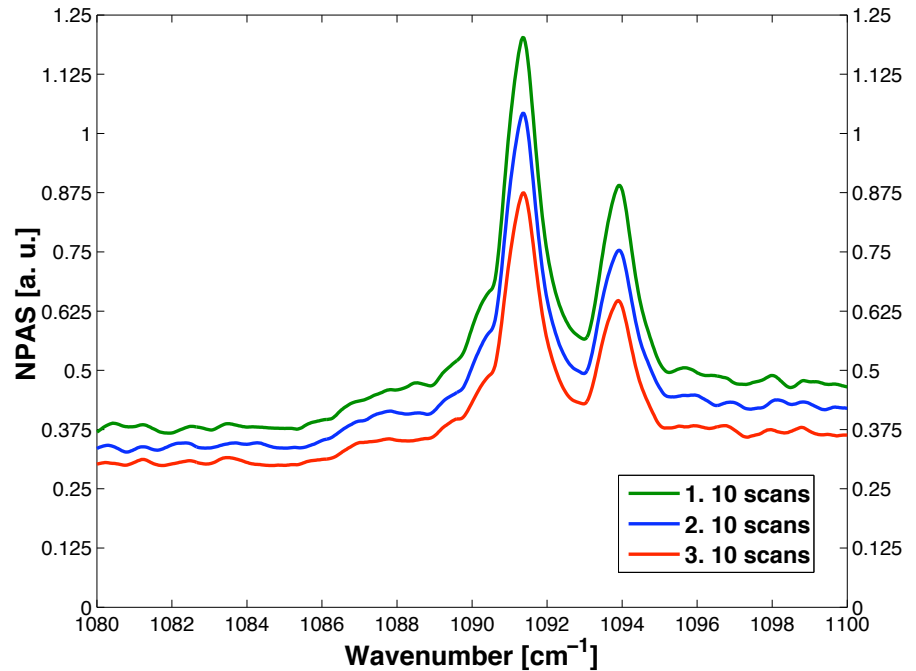
# Monitoring time dependent processes with the QCL

Evaporating drop of glucose solution ( $1077\text{ cm}^{-1}$ )



- The evaporation of the water leads to an increase in glucose concentration

PA spectrum of acetone vapour  $1080\text{-}1100\text{ cm}^{-1}$



- Over time the concentration of acetone in the PA chamber decreases

# Conclusion & Outlook

- Implementation of MIR laser based PA sensor using a double-chamber PA cell closed with a diamond window => strong and stable signals
  - Glucose concentrations within the physiological range detected in aqueous samples
  - Fast tuning of the EC-QCL allows monitoring time-dependent spectral changes between 1000-1100  $\text{cm}^{-1}$
- 
- Measurement in more complex tissue phantoms closer mimicking human tissue
  - Measurement through non-glucose containing layer
  - Including the measurement of different parameters (i.e. temperature, humidity and blood pulsation)
  - *In-vivo* measurements with the PA sensor



Prof. Markus W. Sigrist



Dr. Julien M. Rey

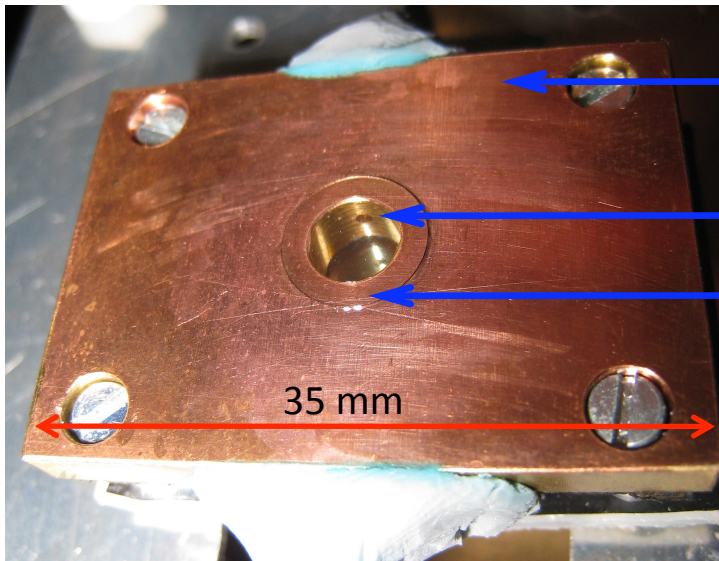


**Sponsoring:**





# Photoacoustic cell

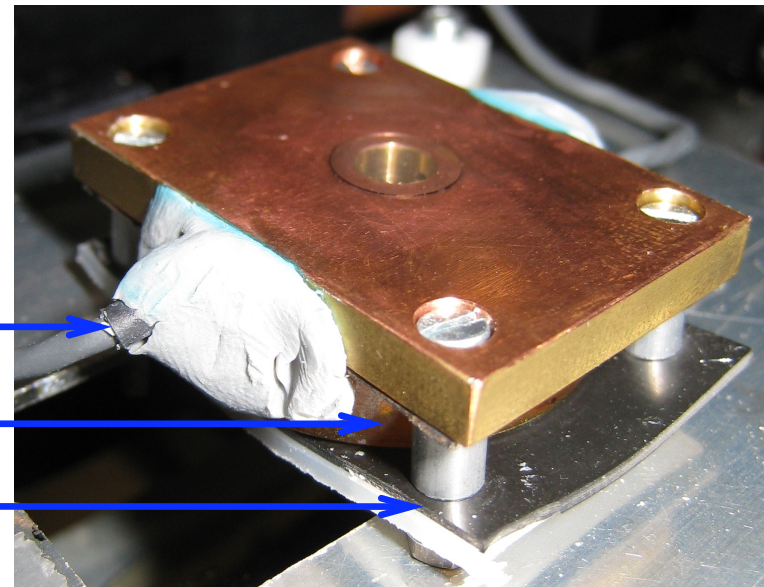


Copper block

Gold coated cell walls and  
connection tube to the microphone

Diamond window

35 mm



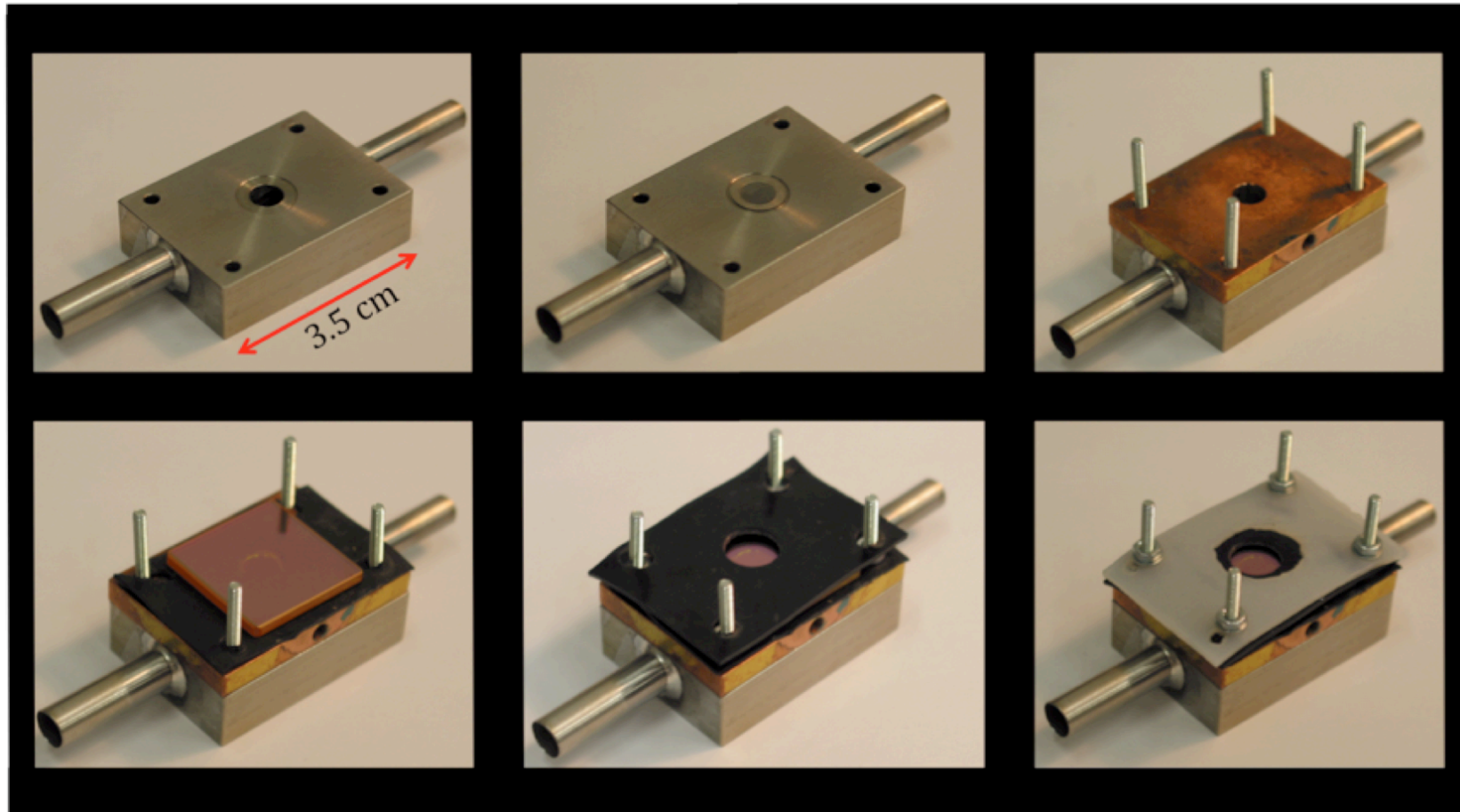
Microphone cable

ZnSe window

Support frame



# Combining the PA cell and the flow cell



# Overview of *in-vivo* Glucose Measurements

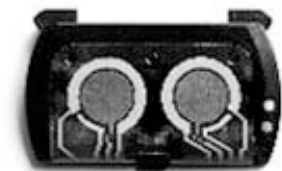
- Making the blood sample-taking more convenient
- Implanted sensors
- Methods of non-invasive glucose measurements:
  - Reverse iontophoresis (GlucoWatch)
  - Optical absorption spectroscopy (NIR and MIR)

## Review:

C. E. F. do Amaral and B. Wolf,  
Medical Engineering & Physics 30(5), 541–549 (2008).



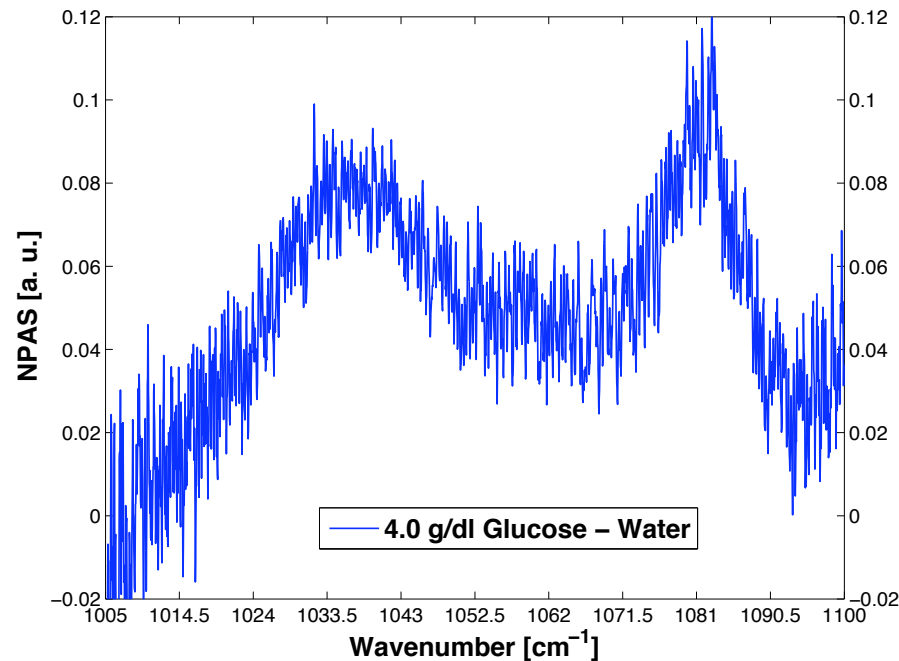
GlucoWatch® Biographer



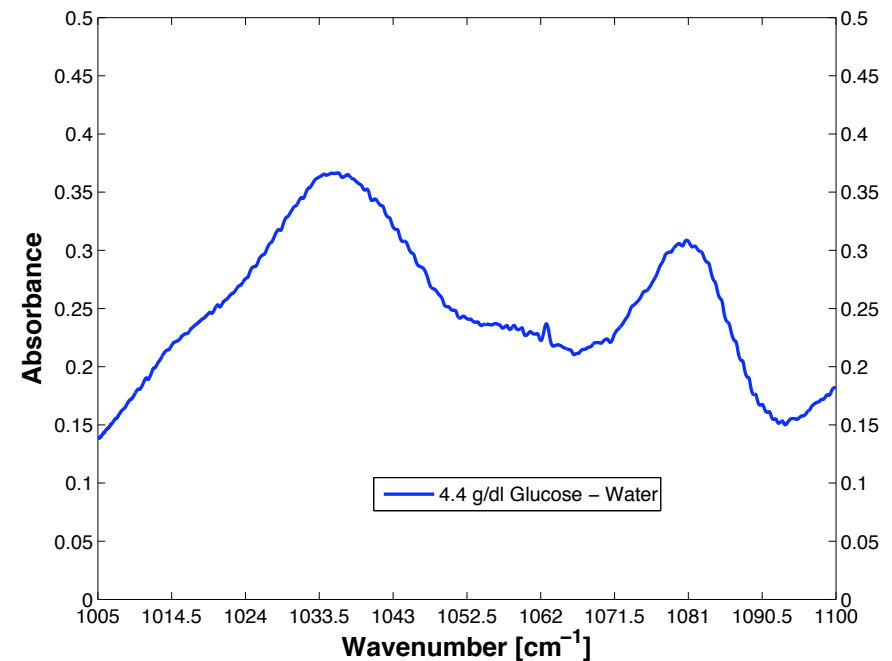
AutoSensor

# Fast recording of a spectrum with the QCL

PA spectrum of glucose 1005-1100  $\text{cm}^{-1}$

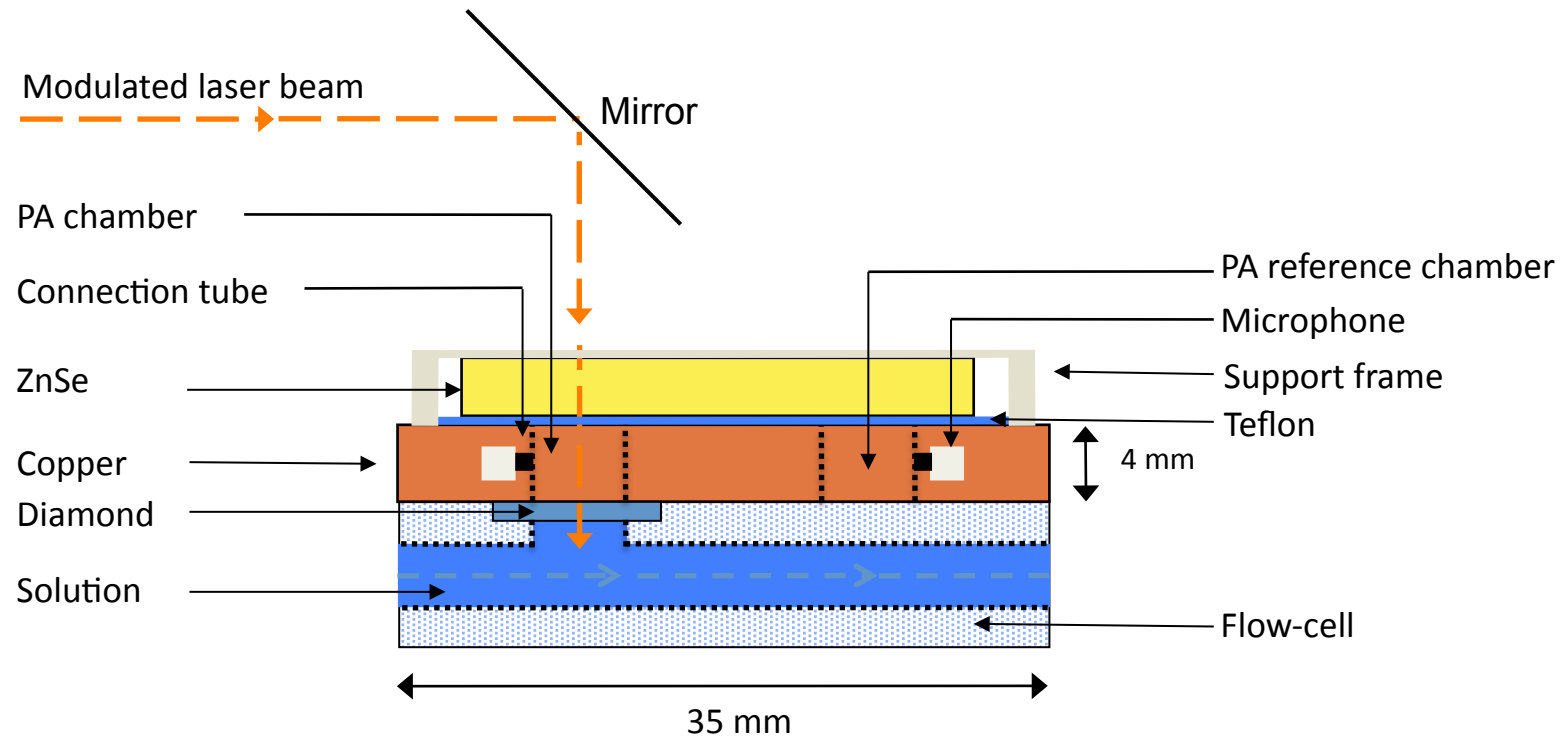


ATR spectrum of glucose 1005-1100  $\text{cm}^{-1}$



- A single spectrum can be recorded within 5.5 s
- An averaging of the single measurement is necessary

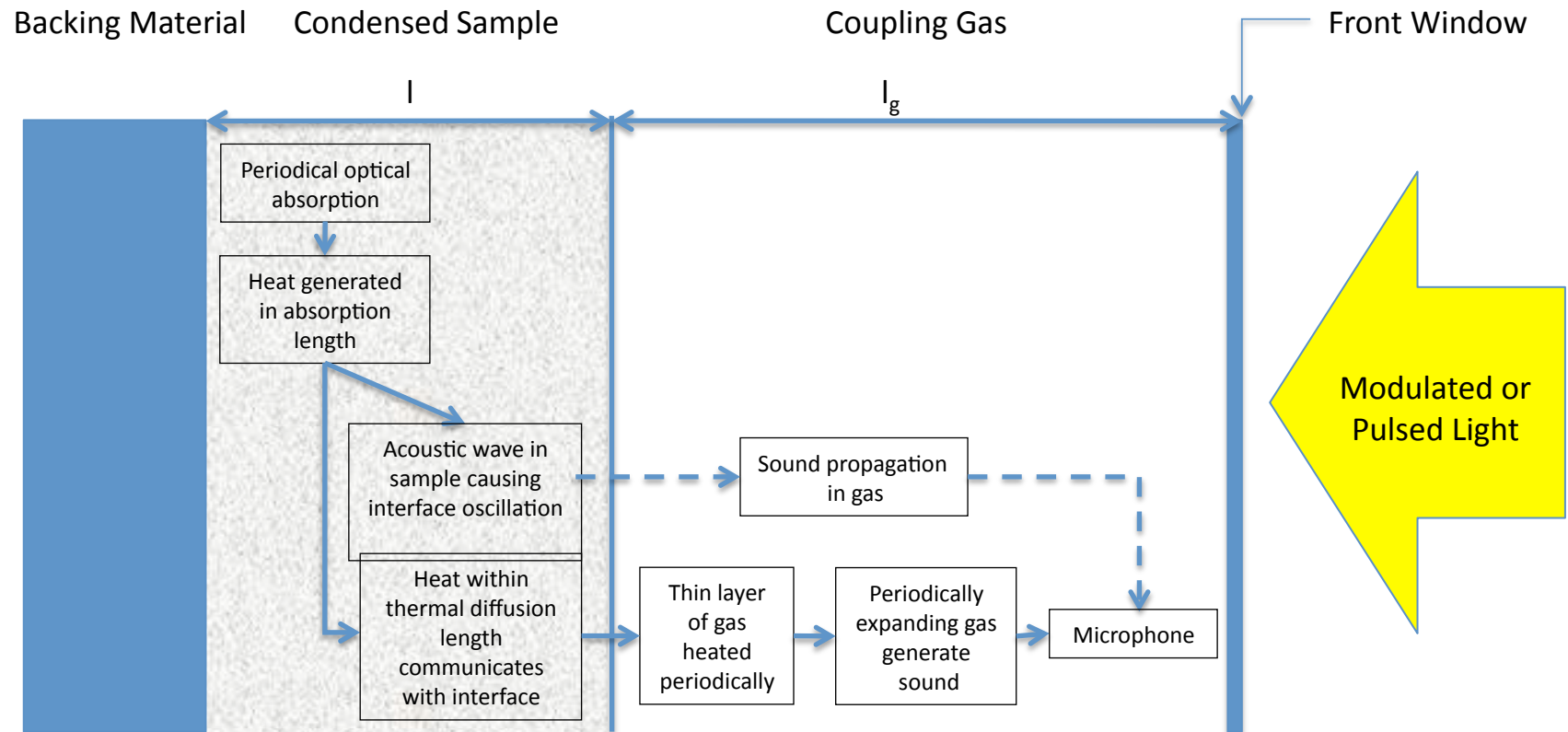
# Photoacoustic cell



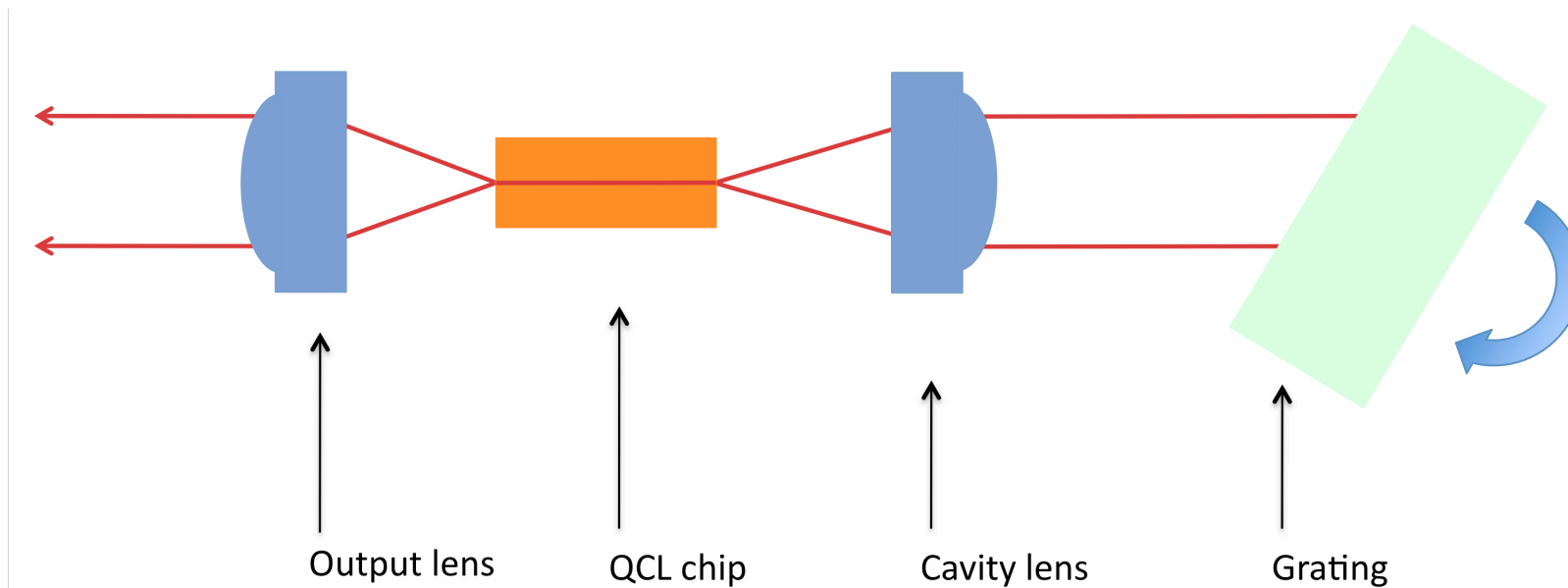
- The glucose concentration can be continuously varied
- Stable measurement conditions
- PA reference chamber for suppression of vibrations and environmental influences
- Pumping can simulate pulsation



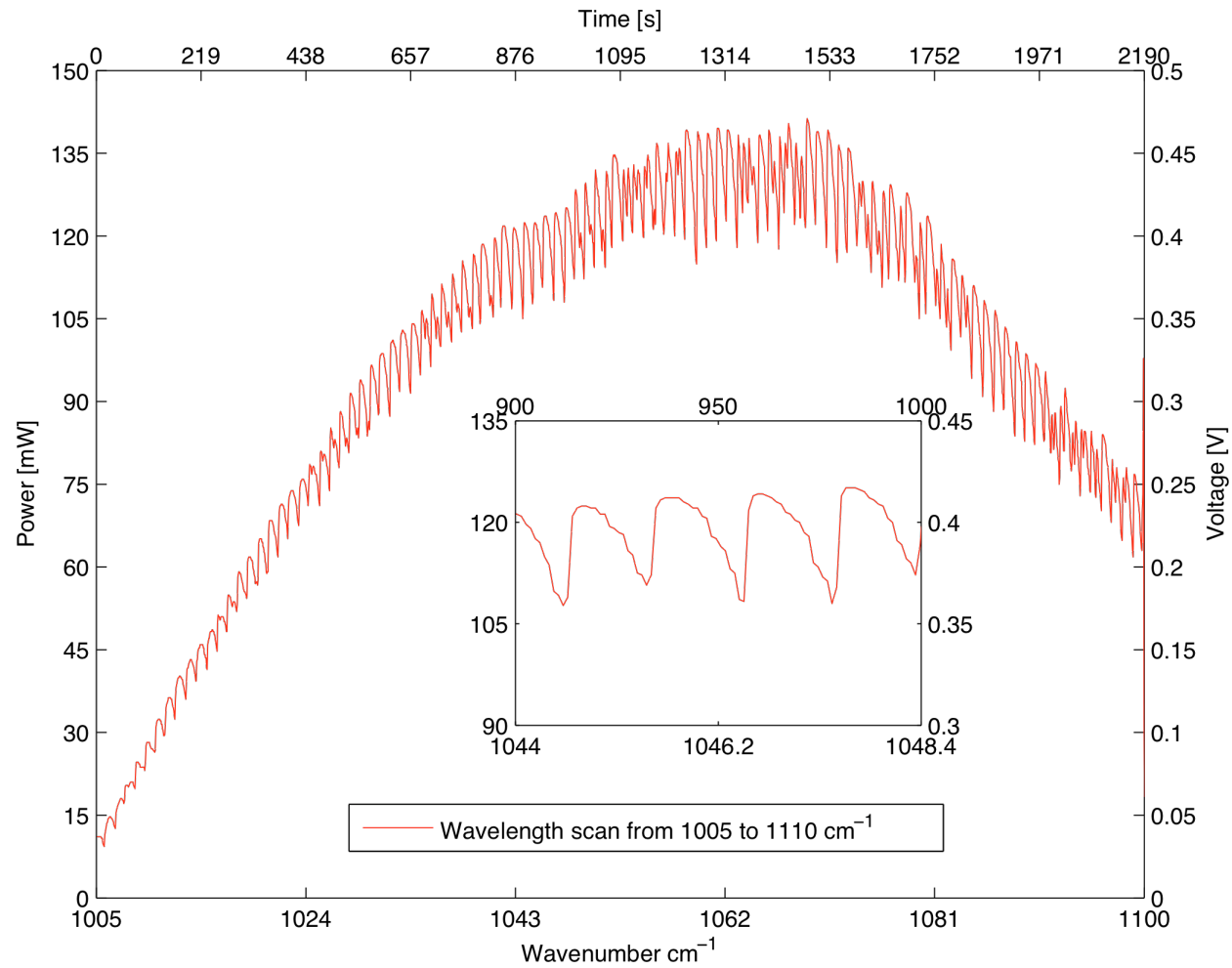
# Gas coupling method



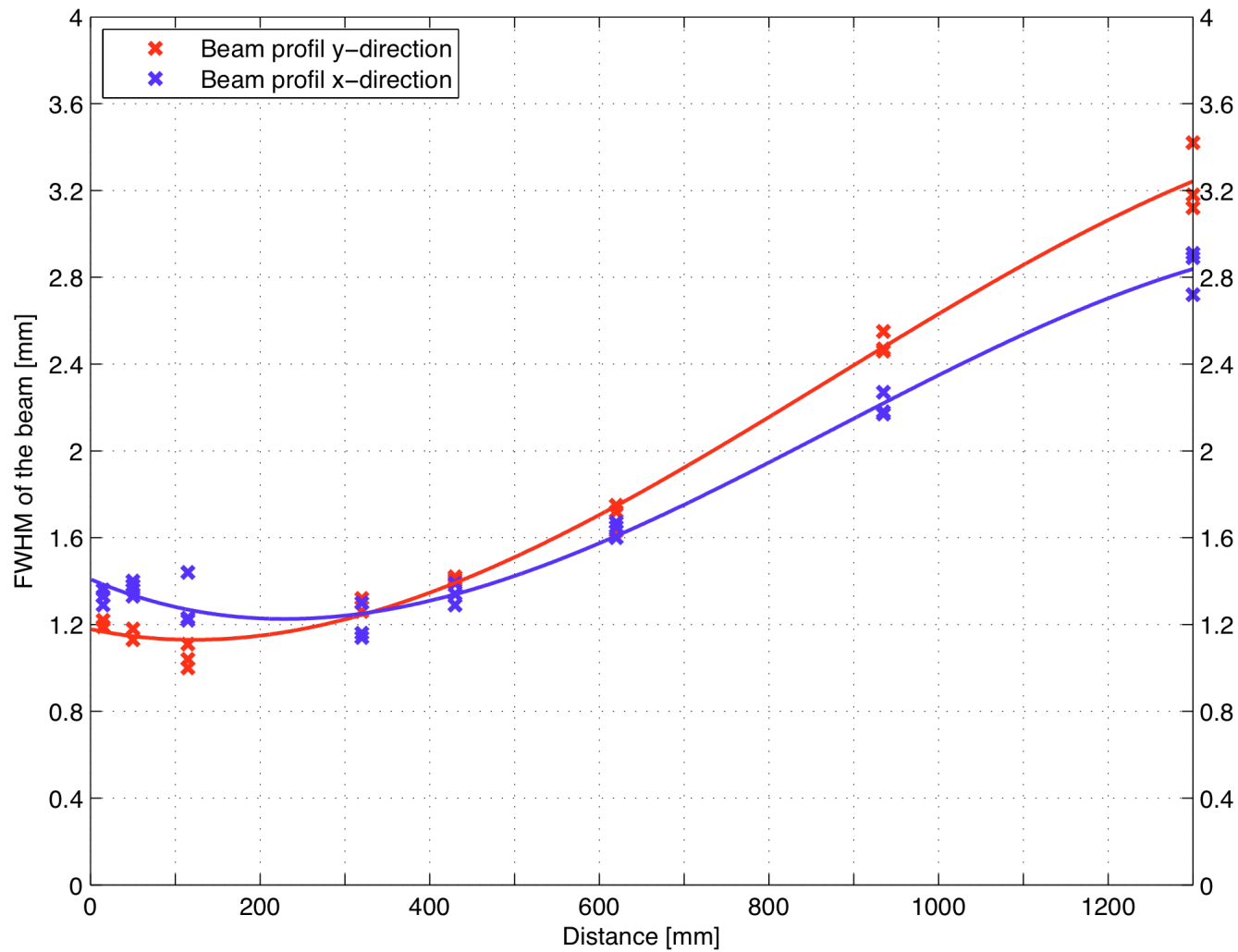
# QCL cavity design



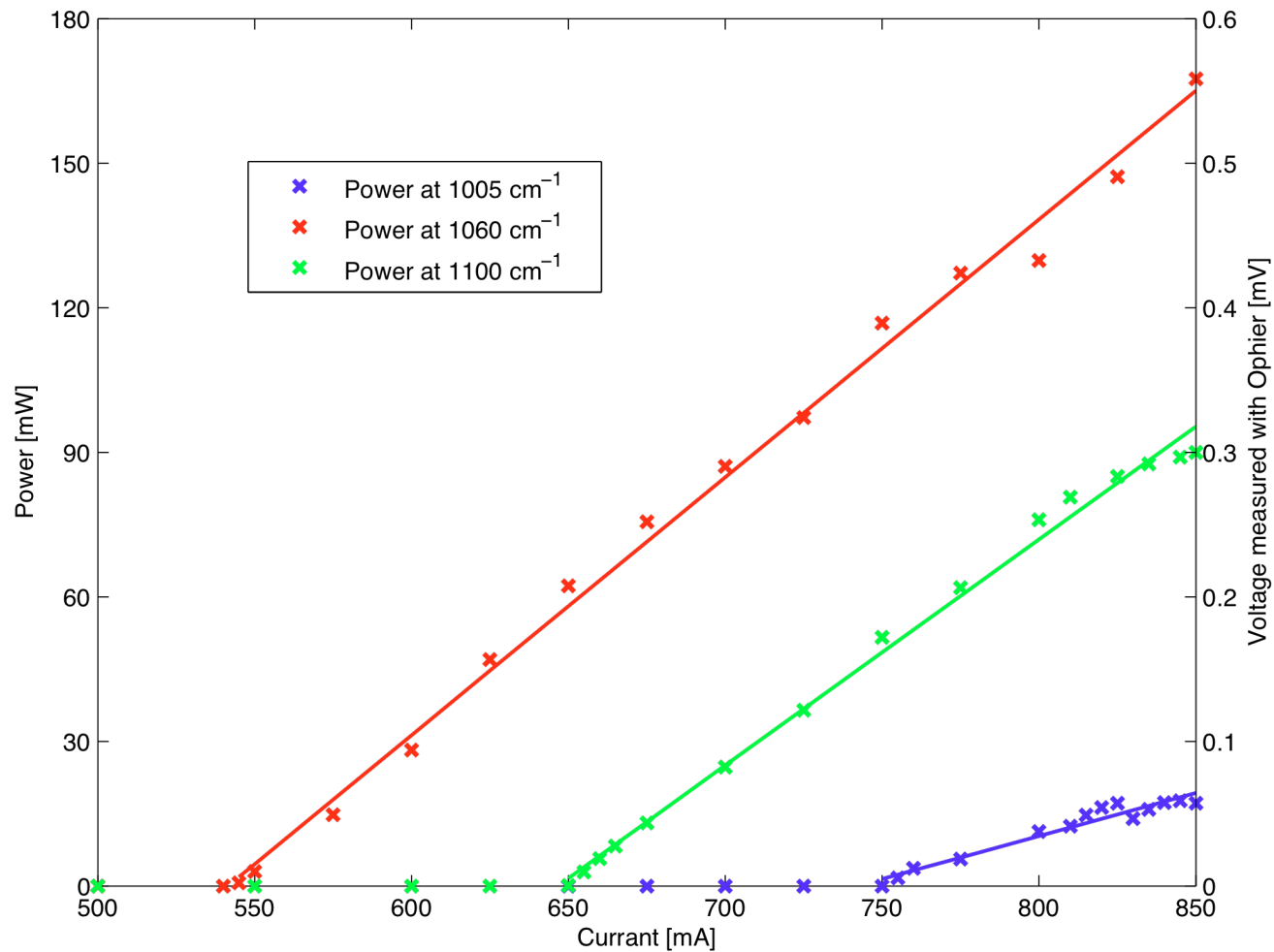
# Power spectrum of the QCL at 800 mA



# FWHM of the QCL beam versus distance from the Laser

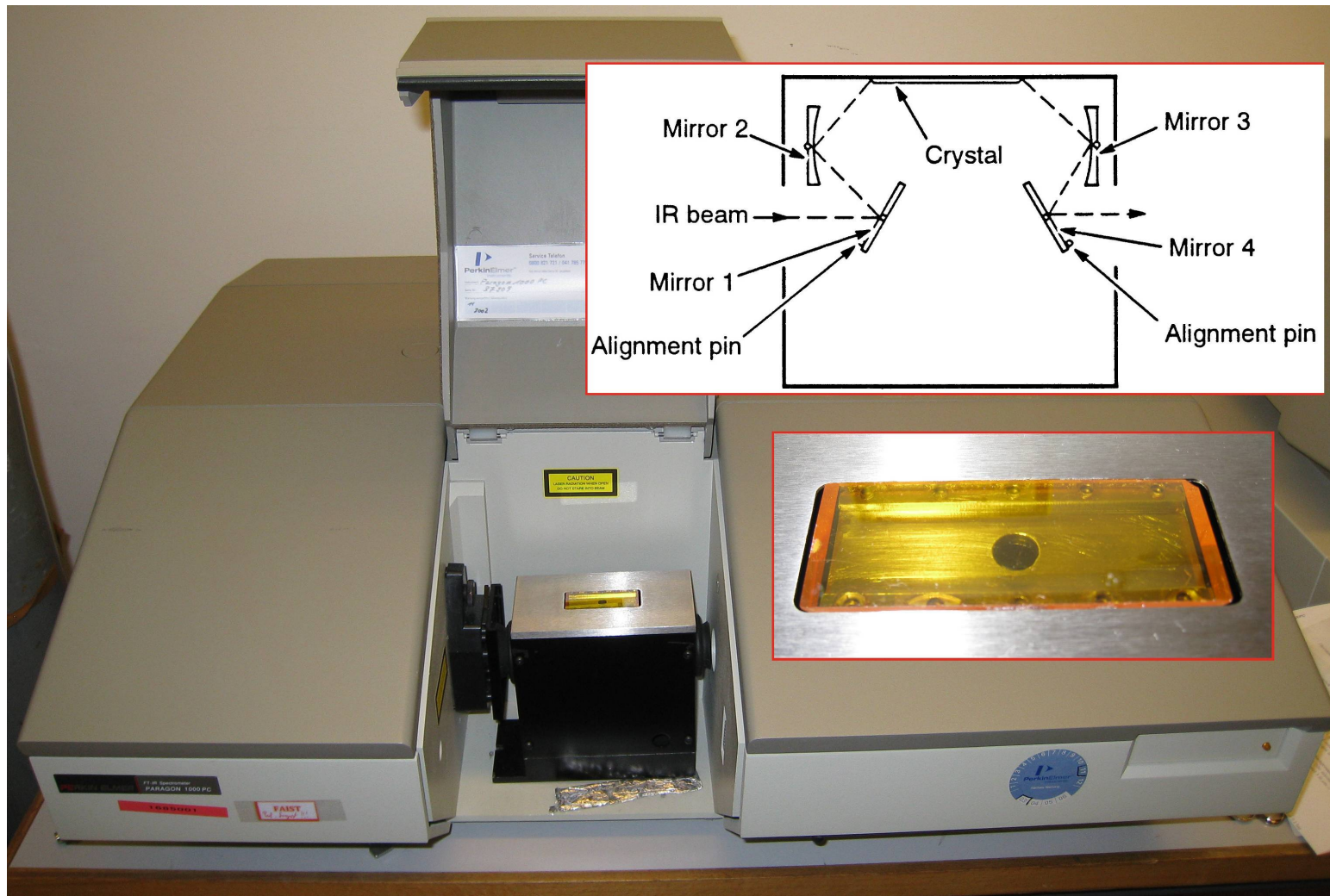


# Output power versus laser current





# FTIR spectrometer with ATR accessory



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- Photoacoustic detection
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